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Exploring continuous and integrated strategies for the up- and downstream processing of human mesenchymal stem cells

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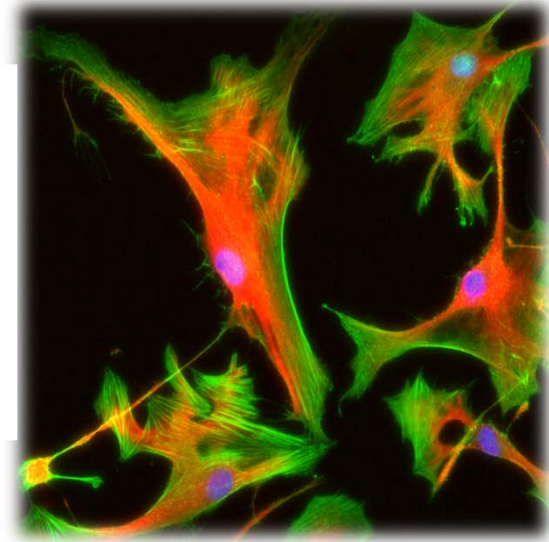
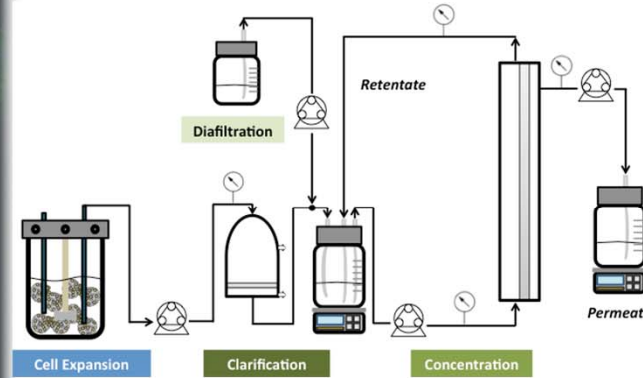
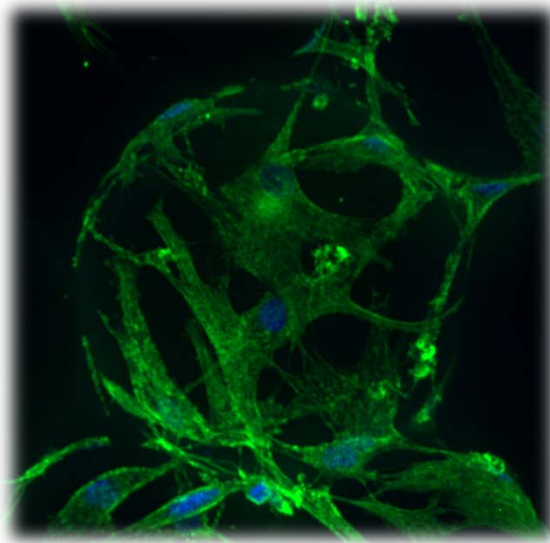
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Authors

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Exploring continuous and integrated strategies for the up- and downstream processing of human mesenchymal stem cells

Paula M. Alves

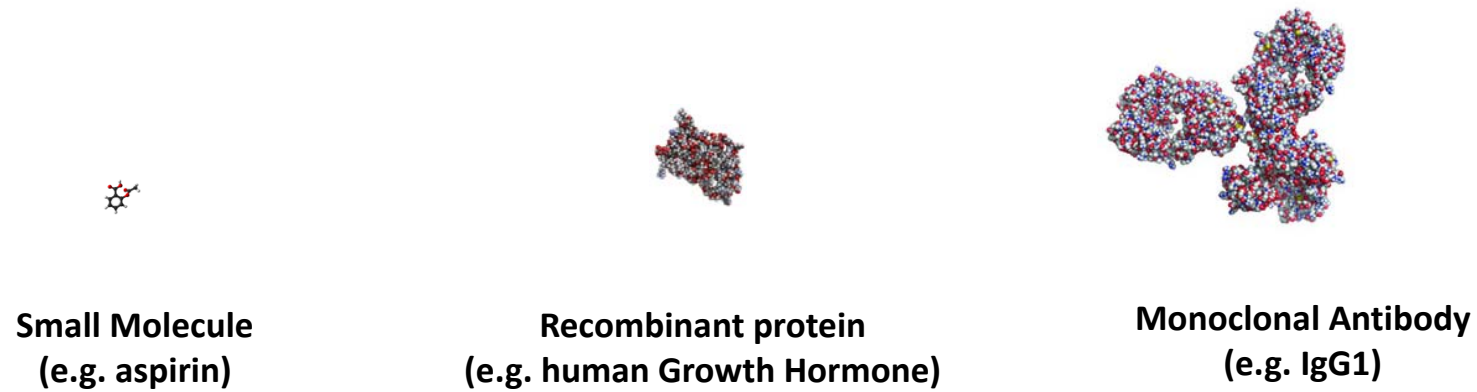
Animal Cell Technology Unit, iBET - Oeiras, Portugal

marques@itqb.unl.pt





Oeiras, Portugal

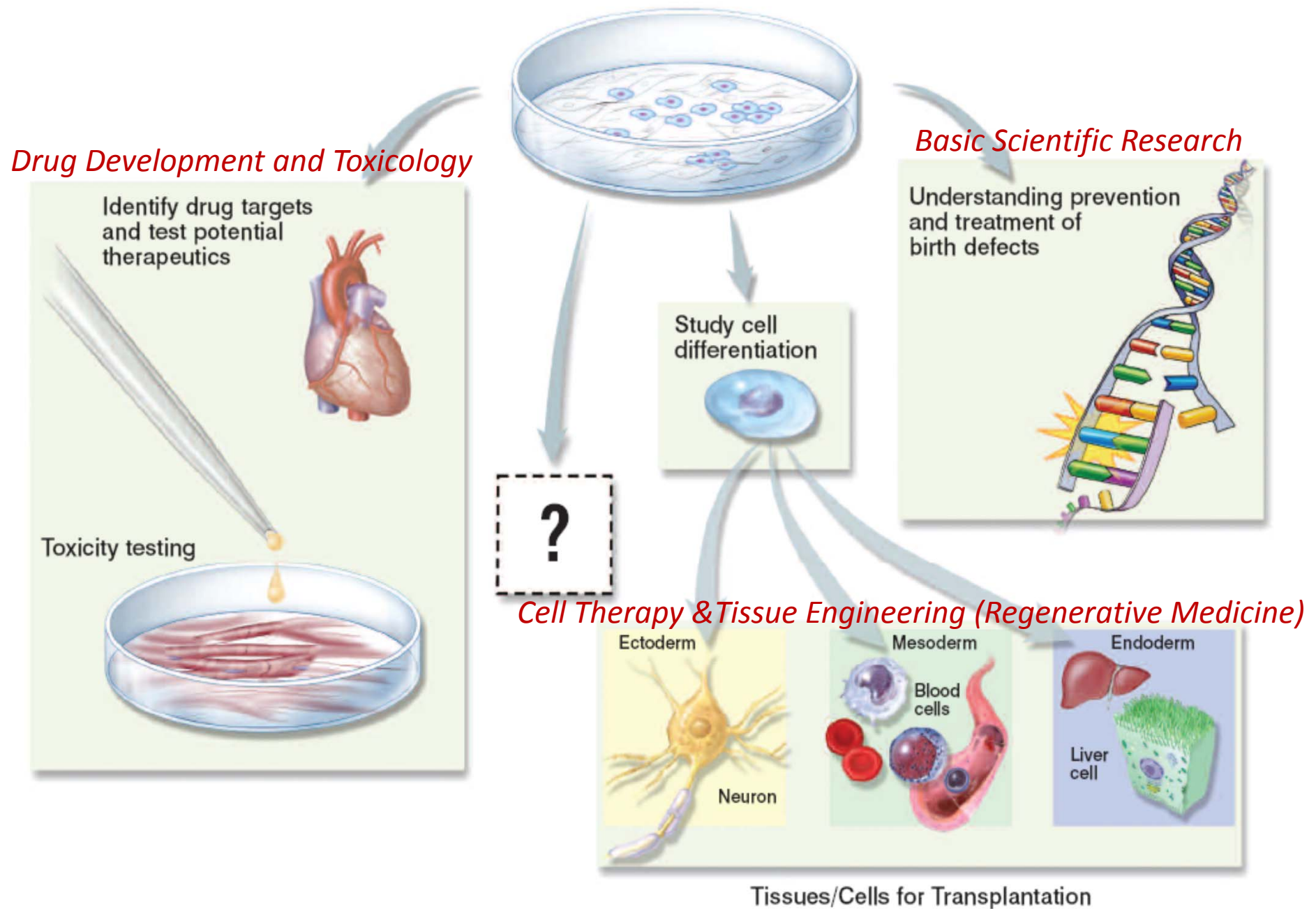


Differences in mass by $\sim 1 \times 10^{12}$

in surface area by $\sim 5 \times 10^6$

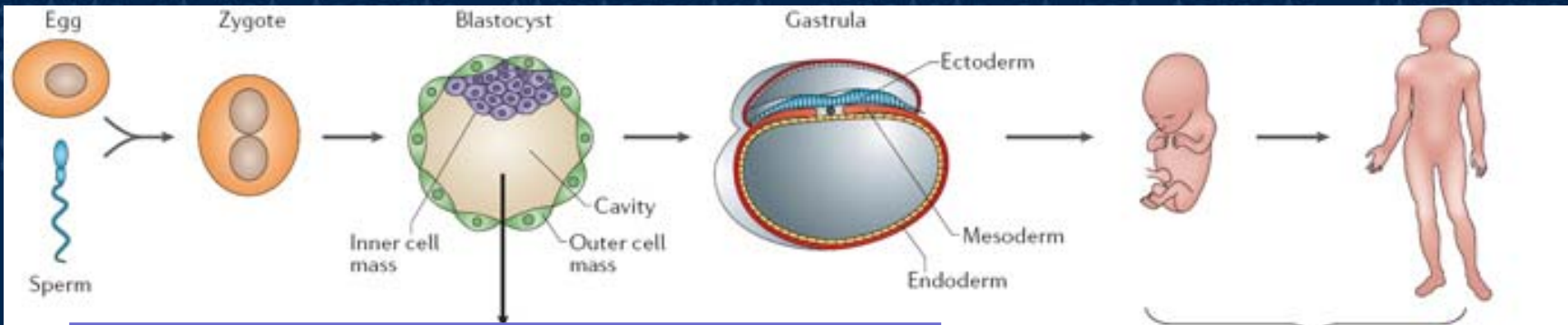


The Promise of Stem Cell Research



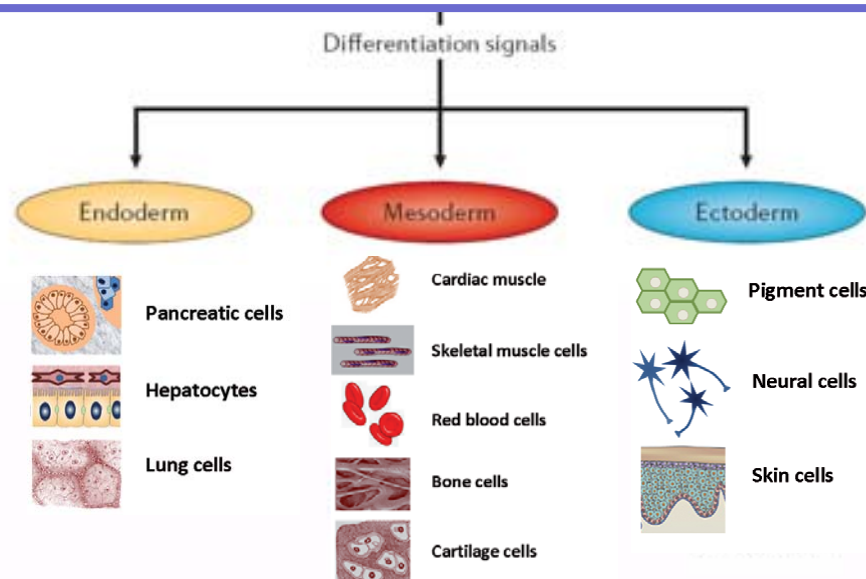
Types

Stem Cells



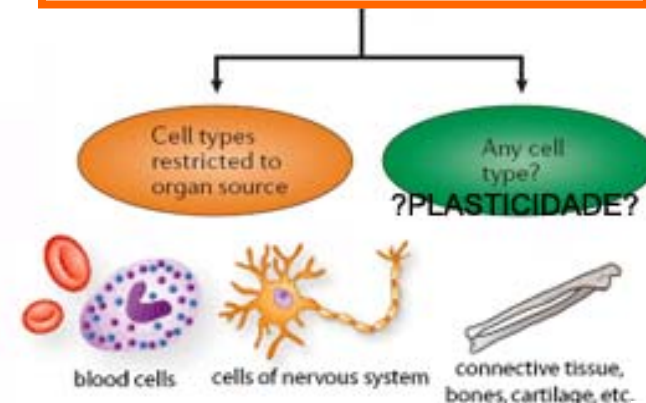
Embryonic Stem Cells (ESCs)

undifferentiated cells derived from a preimplantation embryo (inner cell mass of blastocyst) that are capable of self-renewal, and can develop into cells and tissues of the three primary germ layers



Adult Stem Cells (ASCs)

undifferentiated cells, found in tissues or organs of the body after embryonic development, that are capable of self-renewal and differentiate into specialized cells to replenish dying cells and/or regenerate damaged tissues



Induced Pluripotent Stem Cells (iPSC)

Yamanaka's Lab (Japan)

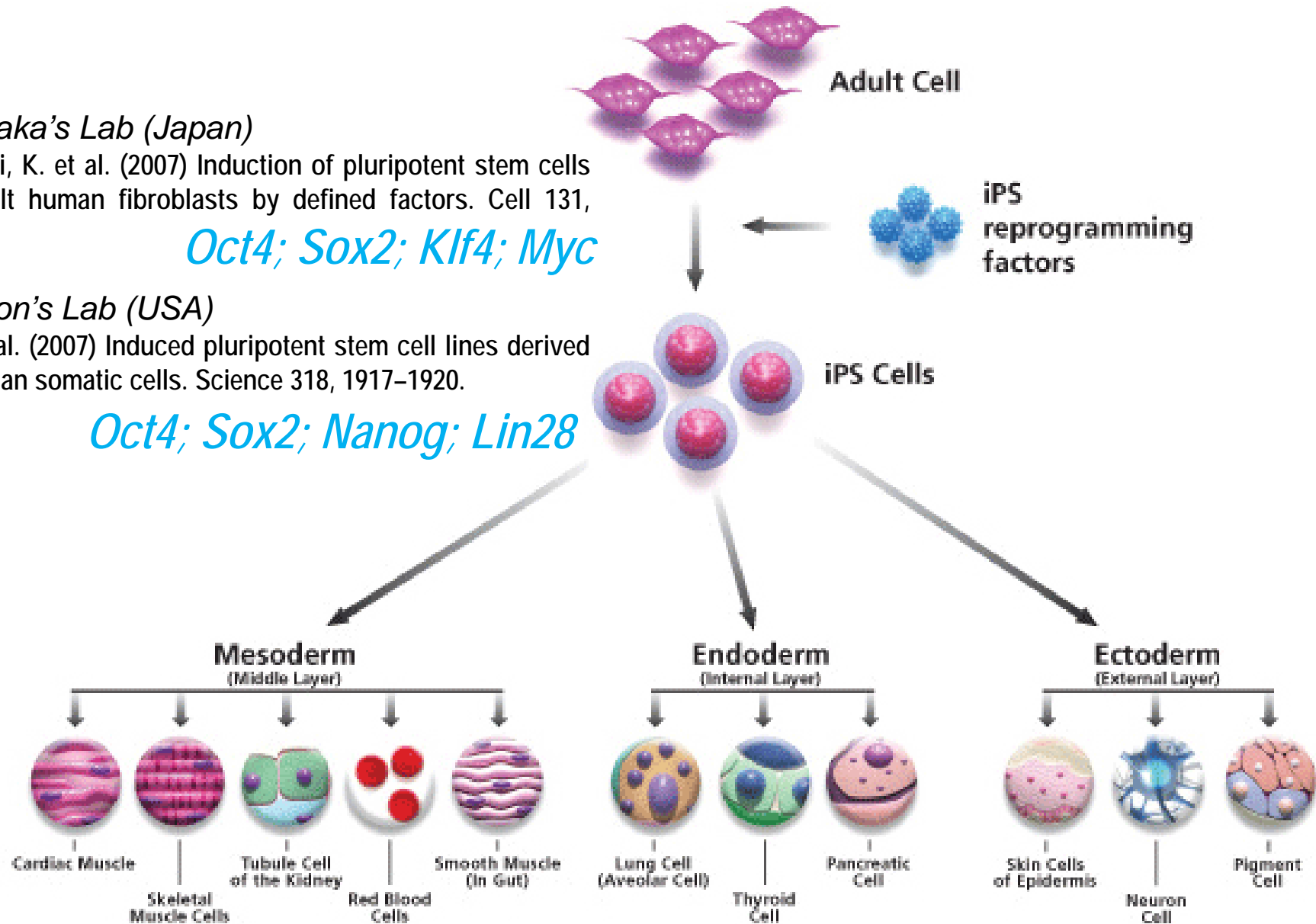
Takahashi, K. et al. (2007) Induction of pluripotent stem cells from adult human fibroblasts by defined factors. Cell 131, 861–872

Oct4; Sox2; Klf4; Myc

Thomson's Lab (USA)

Yu, J. et al. (2007) Induced pluripotent stem cell lines derived from human somatic cells. Science 318, 1917–1920.

Oct4; Sox2; Nanog; Lin28





Clinical trials

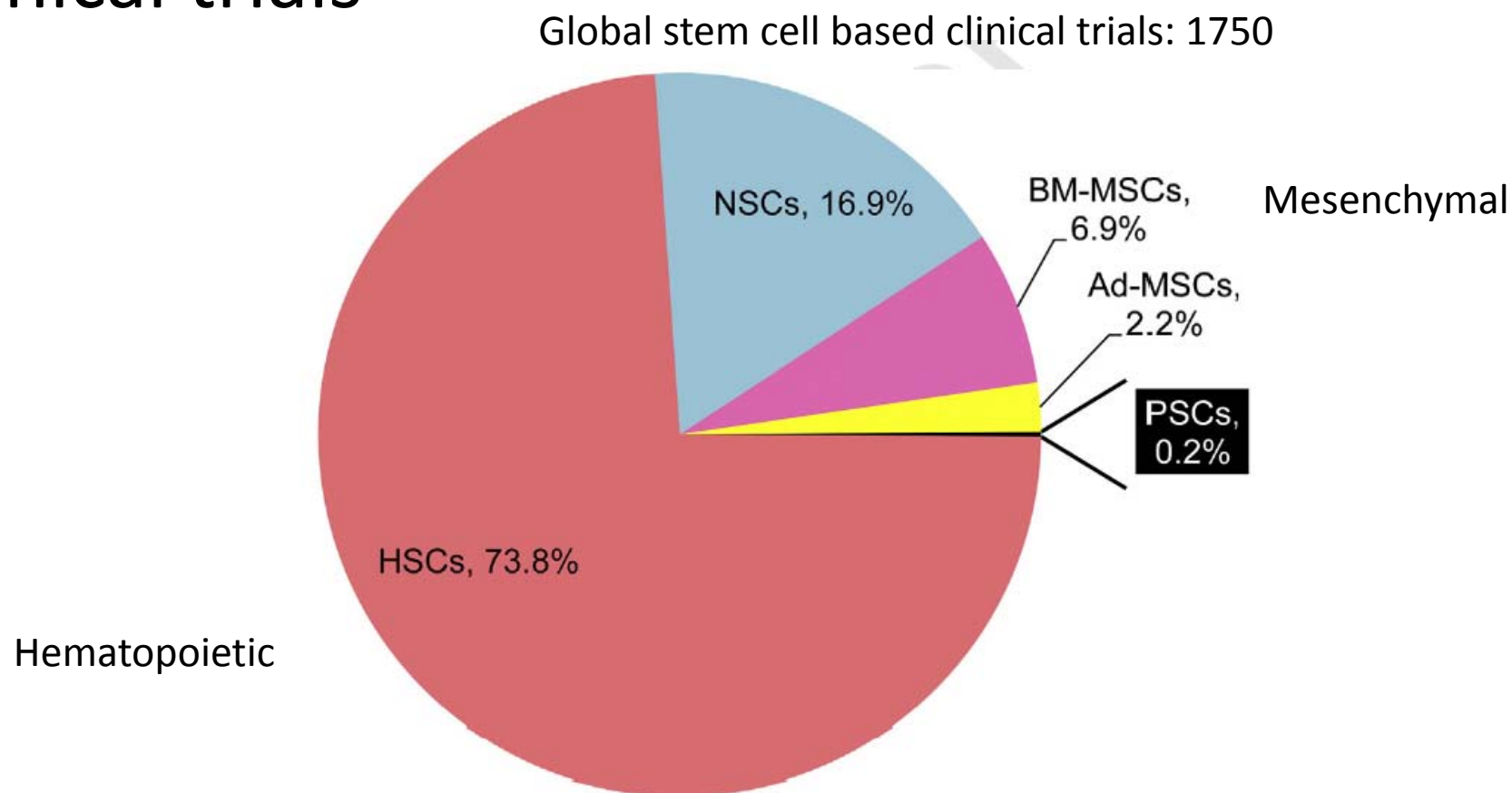


Fig. 1. The share of hPSC based clinical trials in global stem cell based clinical trials at 2012. Pie chart indicating the relative percentage of pluripotent stem cells based clinical trials in total number of open global stem cell based clinical trials (1750 trials) compared to other major stem cell types including hematopoietic (HSCs), neural (NSCs), bone marrow-derived mesenchymal stem cells (BM-MSCs), and adipose-derived MSCs (Ad-MSCs), as extracted from the U.S. NIH website: www.clinicaltrials.gov.

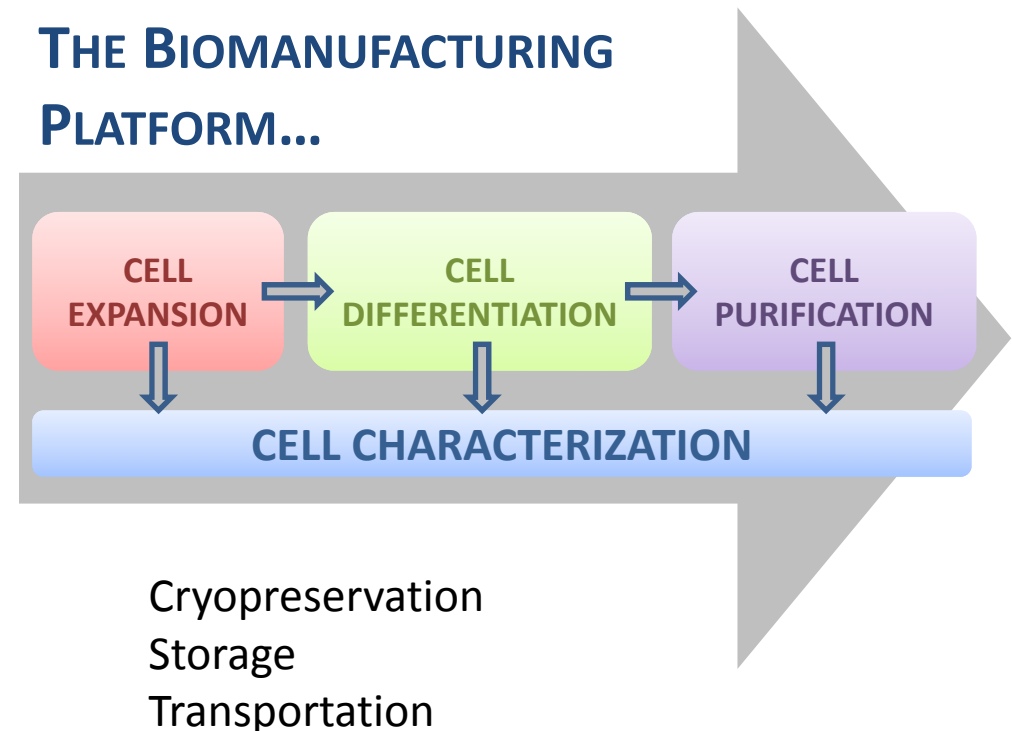


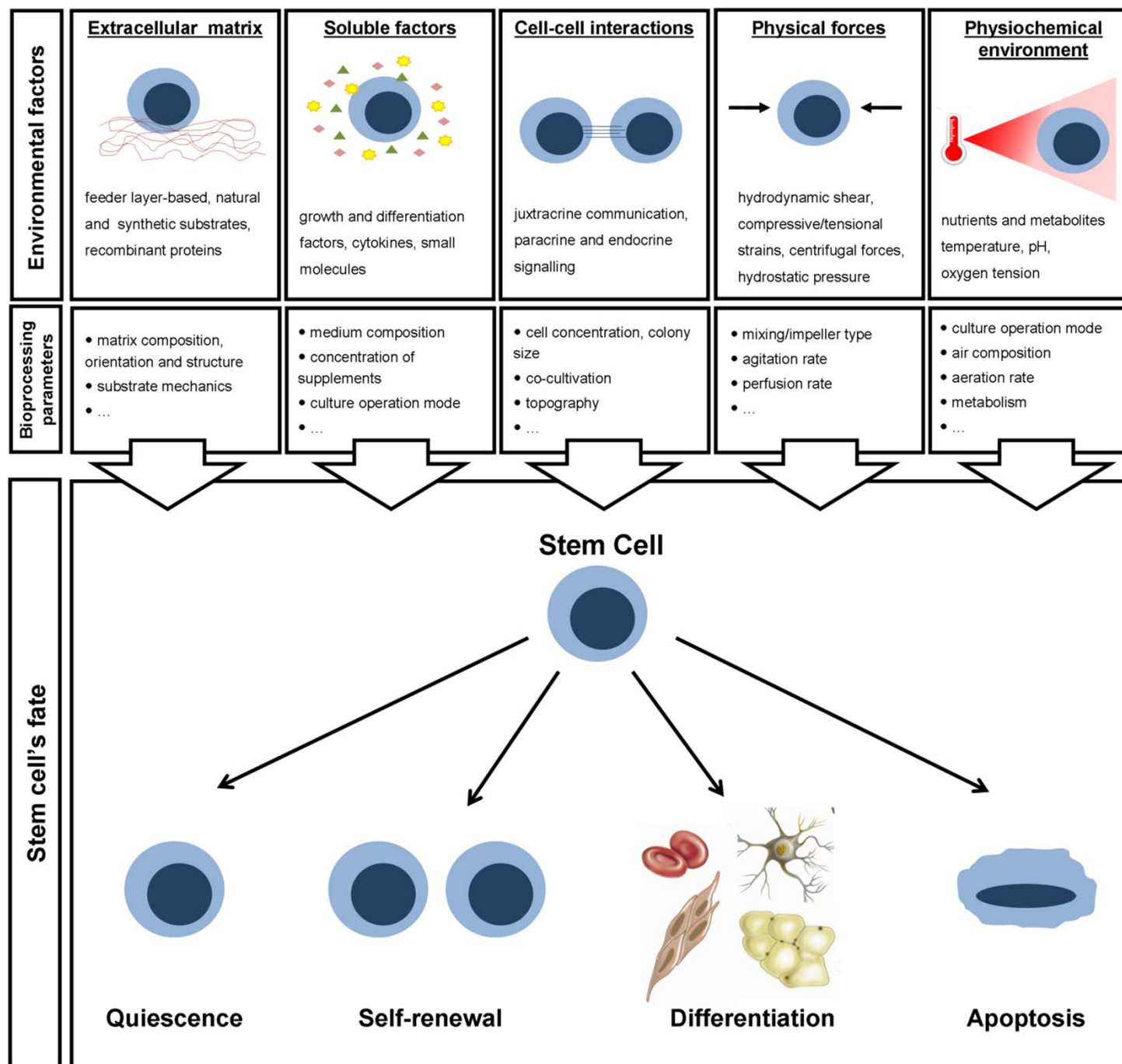
Develop a robust and integrated platform for the production and characterization of challenging stem cell-based products

THE PRODUCT ...



THE BIOMANUFACTURING PLATFORM...

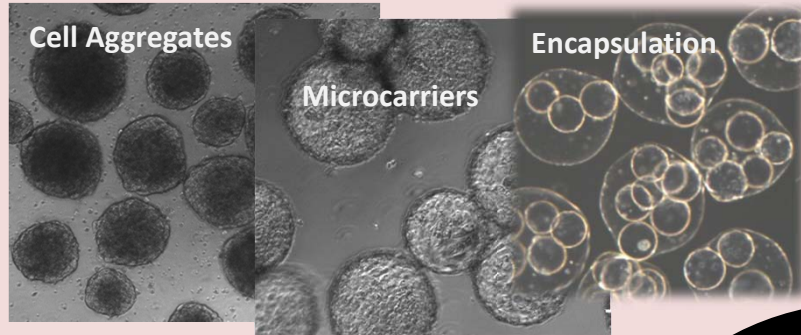




STRATEGY



3D CULTURE SYSTEMS



- ✓ Improve cell viability and function
- ✓ Enhance proliferation/differentiation capacity
- ✓ Preserve 3D cell-cell and cell-matrix contacts
- ✓ Reproducibility and predictability

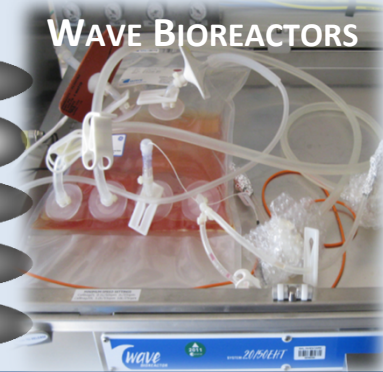
BIOREACTORS

STIRRED TANK BIOREACTORS



- ✓ Scalability
- ✓ Straightforward operation
- ✓ Culture homogeneity
- ✓ Automated
- ✓ Reproducibility
- ✓ Non-destructive sampling
- ✓ cGMP

WAVE BIOREACTORS



Temperature

pO₂

pH

Agitation rate

Perfusion

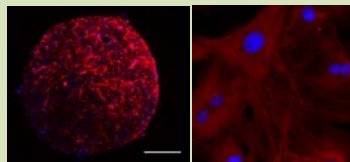
Gas composition

3D
Culture
Systems

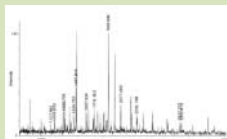
Bioreactors

Cellular
Characterization

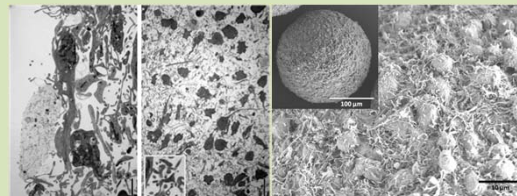
PHENOTYPIC ANALYSIS



PROTEOMIC ANALYSIS



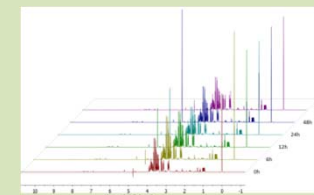
ULTRASTRUCTURE ANALYSIS



TRANSCRIPTOMIC ANALYSIS



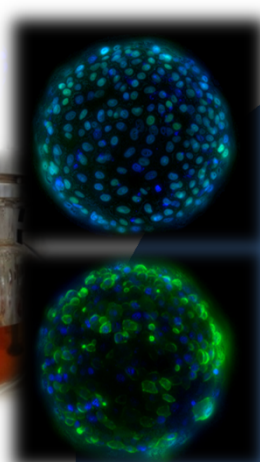
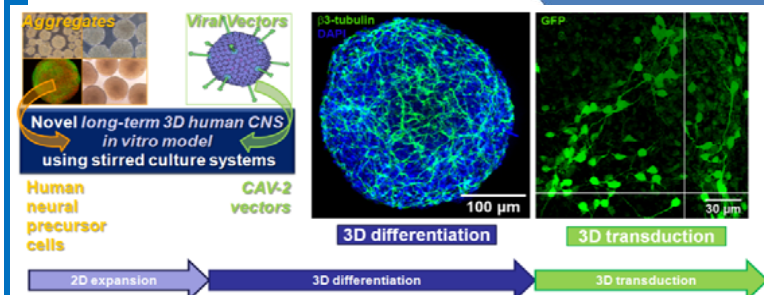
METABOLOMIC ANALYSIS





Serra et al 2010, *J Biotech*;
 Serra/Correia et al 2011, *PLoS ONE*;
 Silva et al 2015, *Stem Cells Transl Med*)

G. Schiavo *Cancer Research UK*;
 J. Schwarz *U Leipzig Germany*,
 E.J. Kremer *GMM, France*



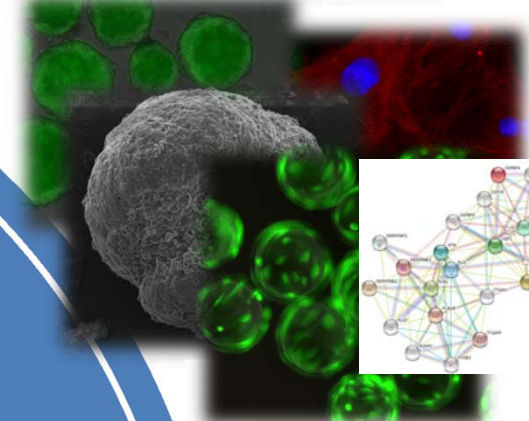
Clinical-grade expansion of hESCs

Production, Purification & Characterization of Cardiomyocytes derived from ESC & iPS cells

Neural differentiation of hNSCs

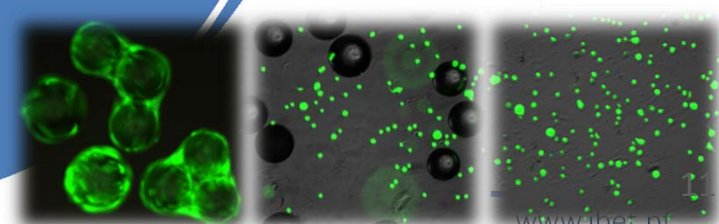
Up- and Down-stream processing of hMSCs

Gomes-Alves et al 2014, *Proteomics*



Serra et al 2012, *Trends in Biotech*;
 Correia et al 2014, *Stem Cell Rev Rep*;

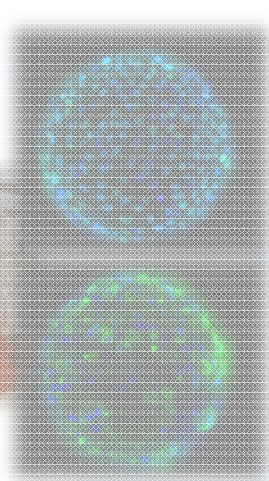
Cunha et al 2015, *J Membr Sci*;
 Cunha et al 2015, *J Biotech*;
 Sousa et al 2015, *Biotechnol Prog*



Gomes-Alves et al 2014, Proteomics

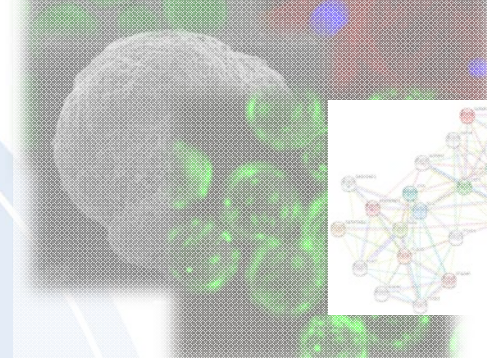


Serra et al 2010, J Biotech;
Serra/Correia et al 2011, PLoS ONE;
Silva et al 2015, Stem Cells Transl Med)



Clinical-grade
expansion of
hESCs

Production,
Purification &
Characterization
of
Cardiomyocytes
derived from
CSC & iPS cells



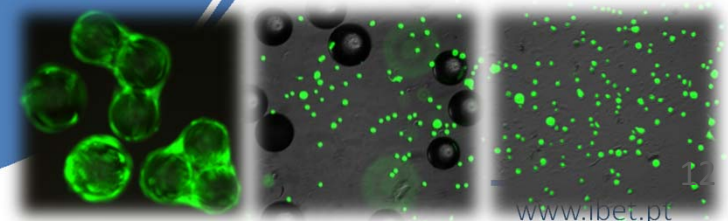
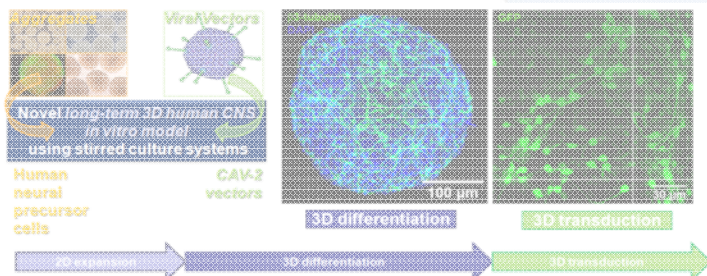
Serra et al 2012, Trends in Biotech;
Correia et al 2014, Stem Cell Rev Rep;

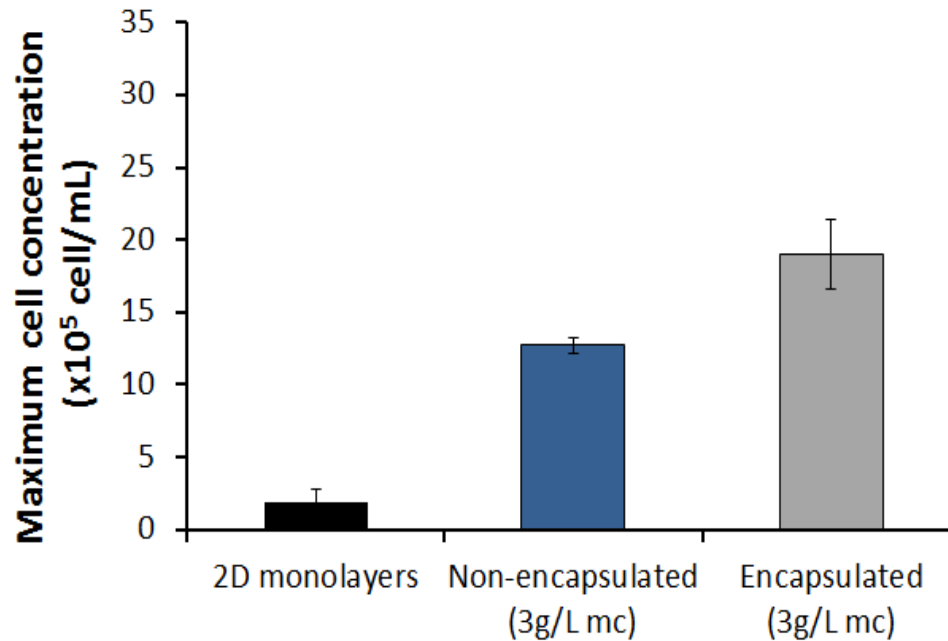
G. Schiavo **Cancer Research UK**;
J. Schwarz **U Leipzig Germany**,
E.J. Kremer **GMM, France**

Neural
differentiation
of **hNSCs**

Up- and Down-
stream
processing of
hMSCs

Cunha et al 2015, J Membr Sci;
Cunha et al 2015, J Biotech;
Sousa et al 2015, Biotechnol Prog



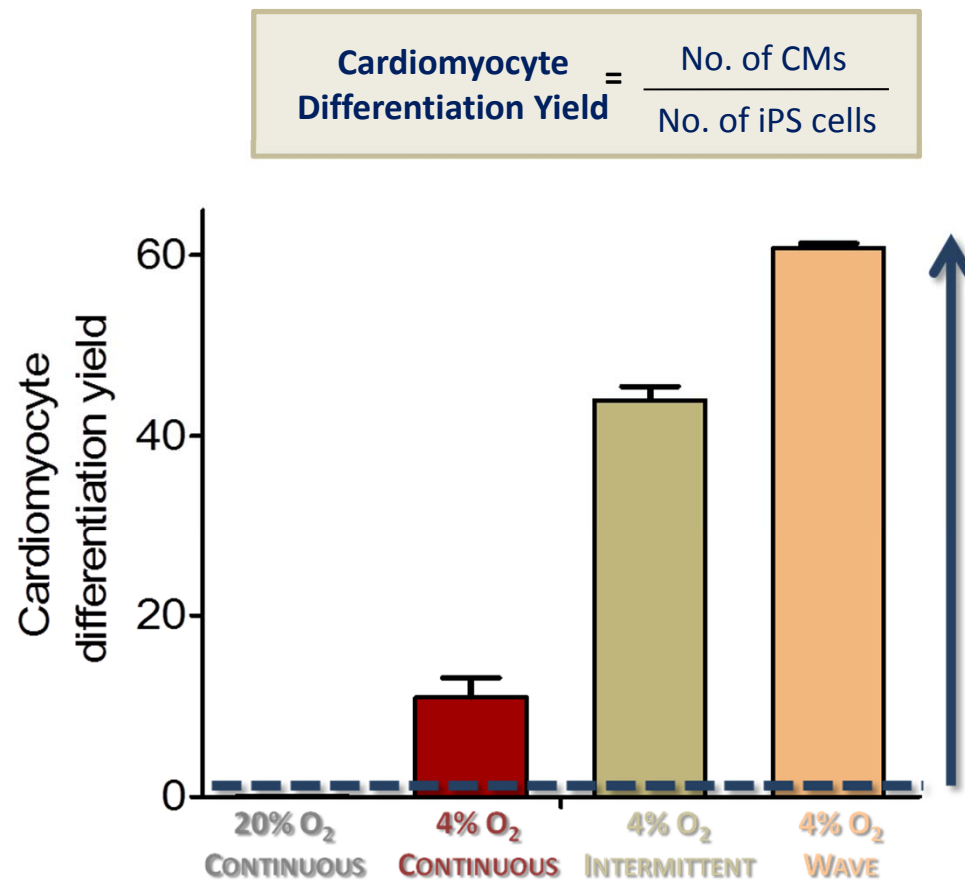
**Expansion**

Higher Volumetric Productivities (up to 10x)

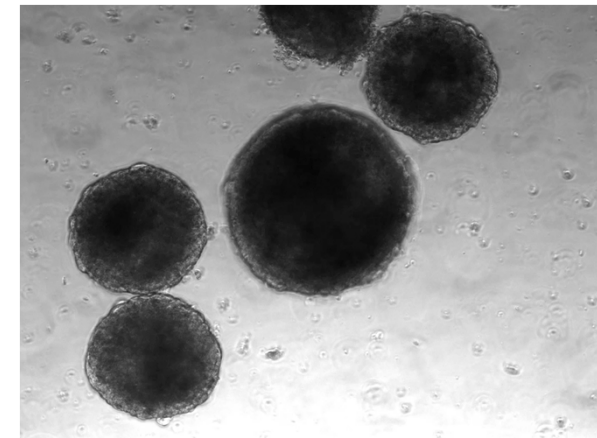
avoiding spontaneous differentiation



The use of environmentally controlled bioreactors is critical to ensure **EFFICIENT** and **SCALABLE** production of functional cardiomyocytes derived from induced pluripotent stem cells



Correia et al., 2014



**>1000-FOLD
IMPROVEMENT**

2.3 x10⁹ CMs
per 1L bioreactor run

human 3D neural models @ iBET : Strategy

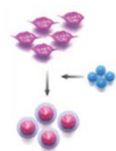
Human Neural Cell Sources:



Human Embryonic Stem Cells (hESC) & Embryonal Carcinoma Stem Cells



Human fetal Neural Stem Cells (hNSC)

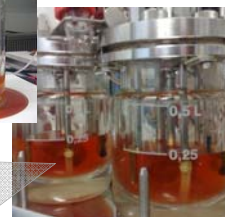


Induced Pluripotent Stem Cells (iPSC)

Continuous Perfusion Stirred Tank Bioreactors:



Systems: DasGip, BIOSTAT Qplus (Sartorius)

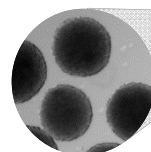


• **Working volumes:**

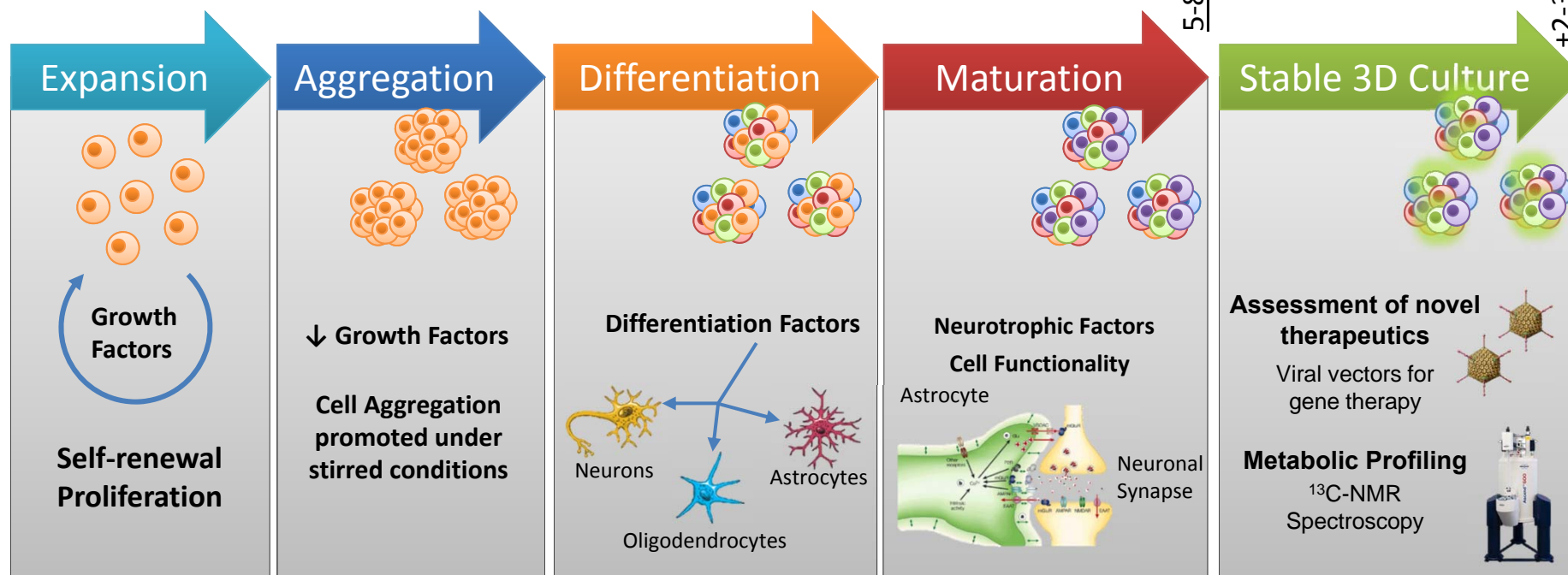
100-500 mL

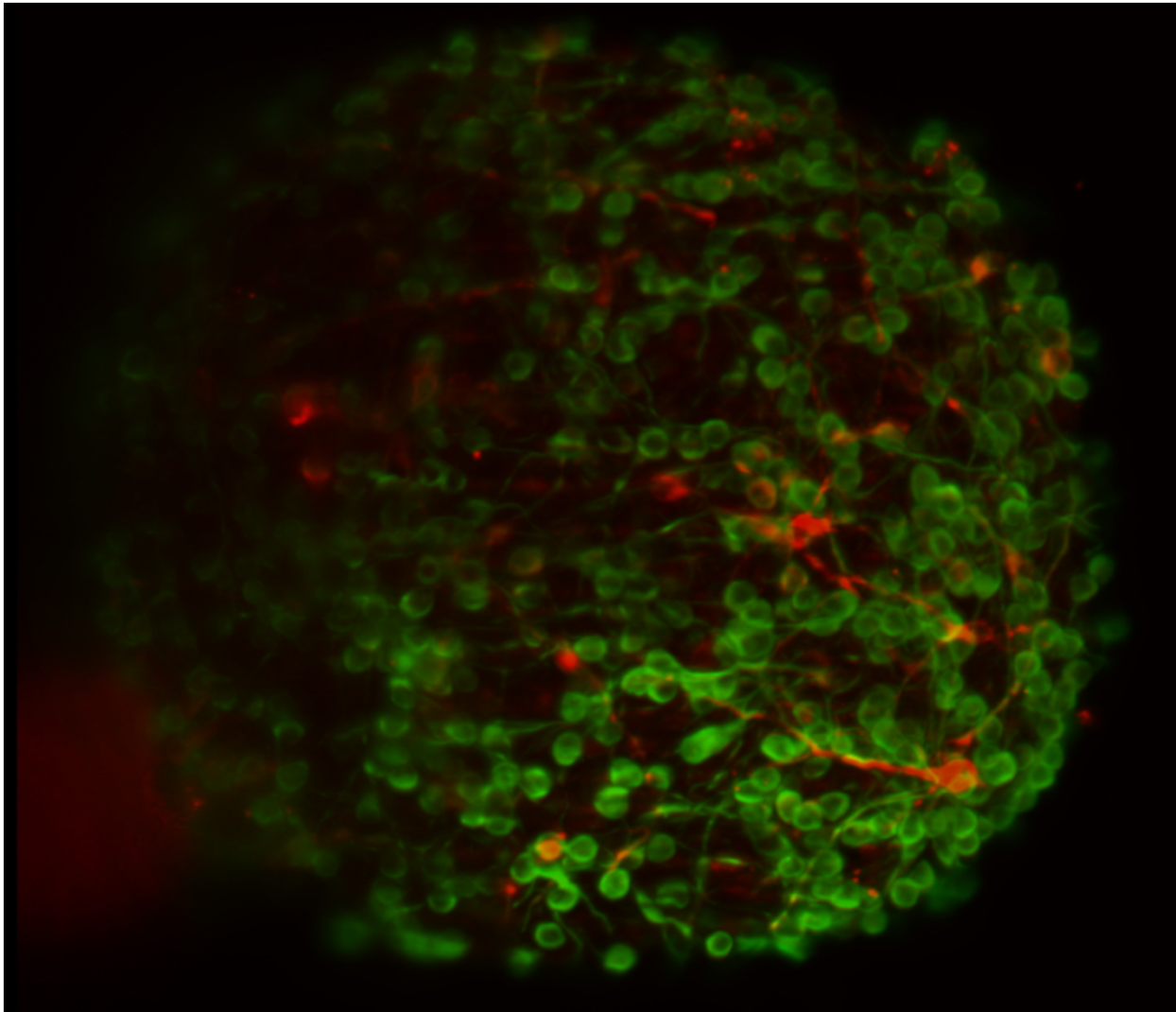
• **Low Oxygen Tensions:**

pO_2 = 15-25% (Air Saturation)



neurospheres



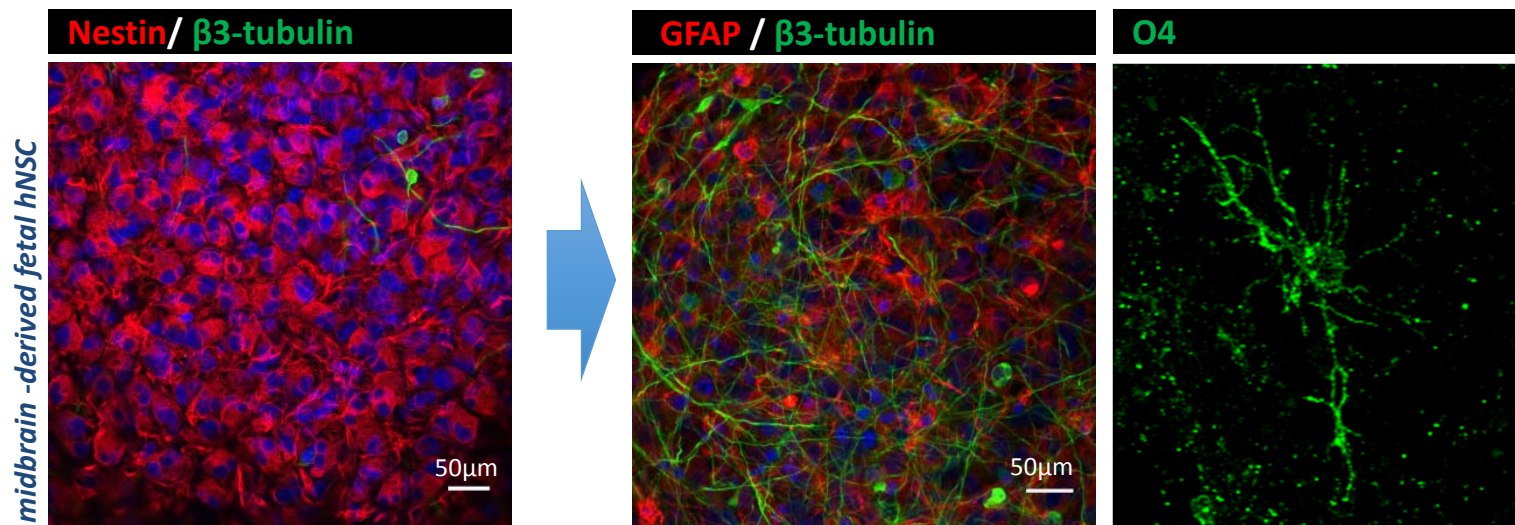


✓ Differentiated neurospheres enriched in DOPAmnergic neuronal markers

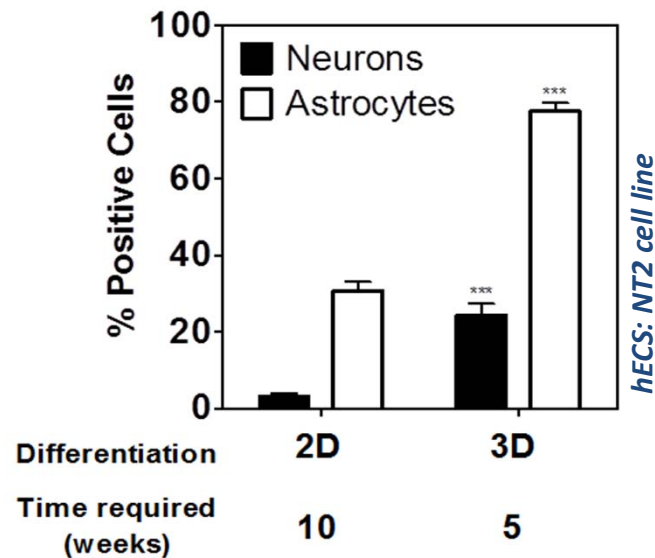
βIII-tubulin

TH – Tyrosine Hydroxylase

Neuronal and glial 3D differentiation



Differentiation Yield



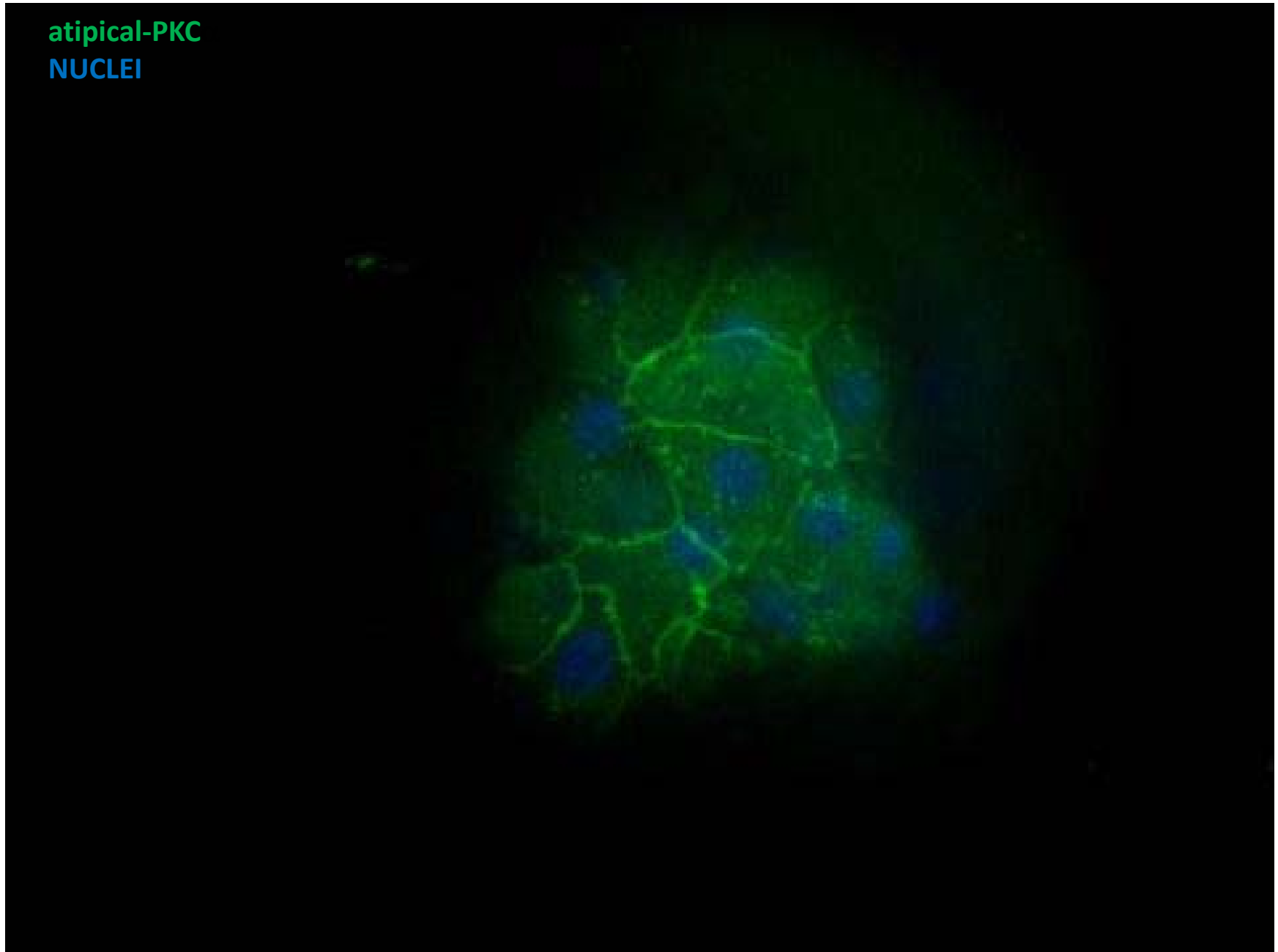
Enrichment in cells from the 3 neural lineages:

- ✓ **Neurons (β III-tub)**
- ✓ **Astrocytes (GFAP)**
- ✓ **Oligodendrocytes (O4)**

3D differentiation process:

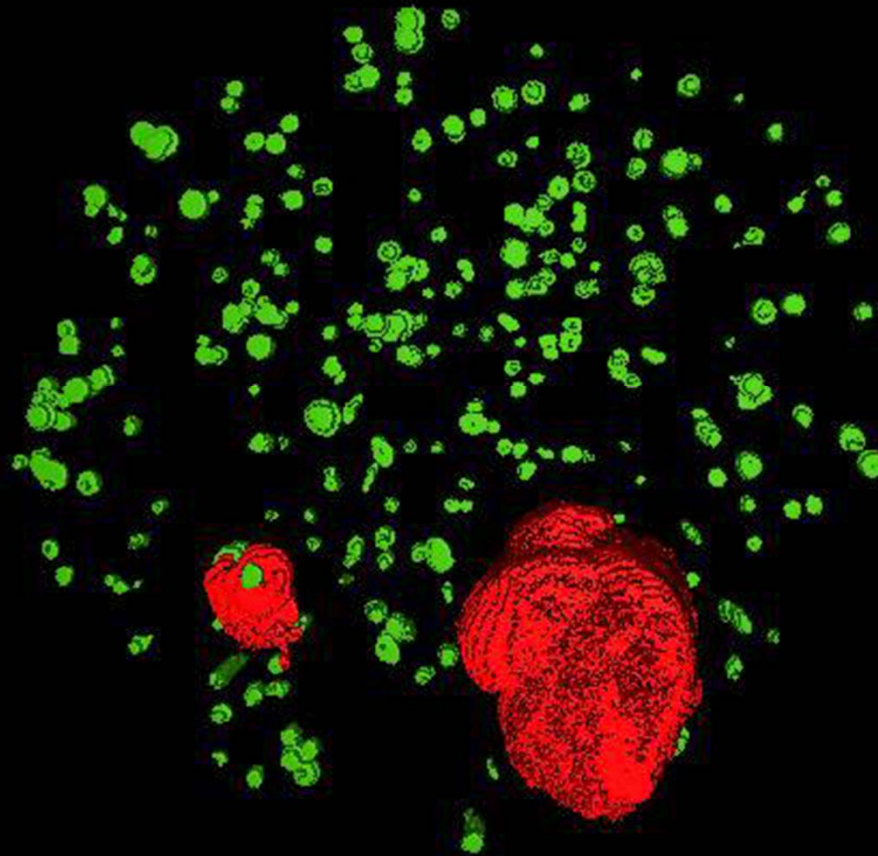
- ✓ **Higher differentiation efficiency**
- ✓ **Less time consuming process**

atypical-PKC
NUCLEI



MICROENVIRONMENT RECAPITULATION: ENCAPSULATION

Co-culture of tumour spheroids with fibroblast



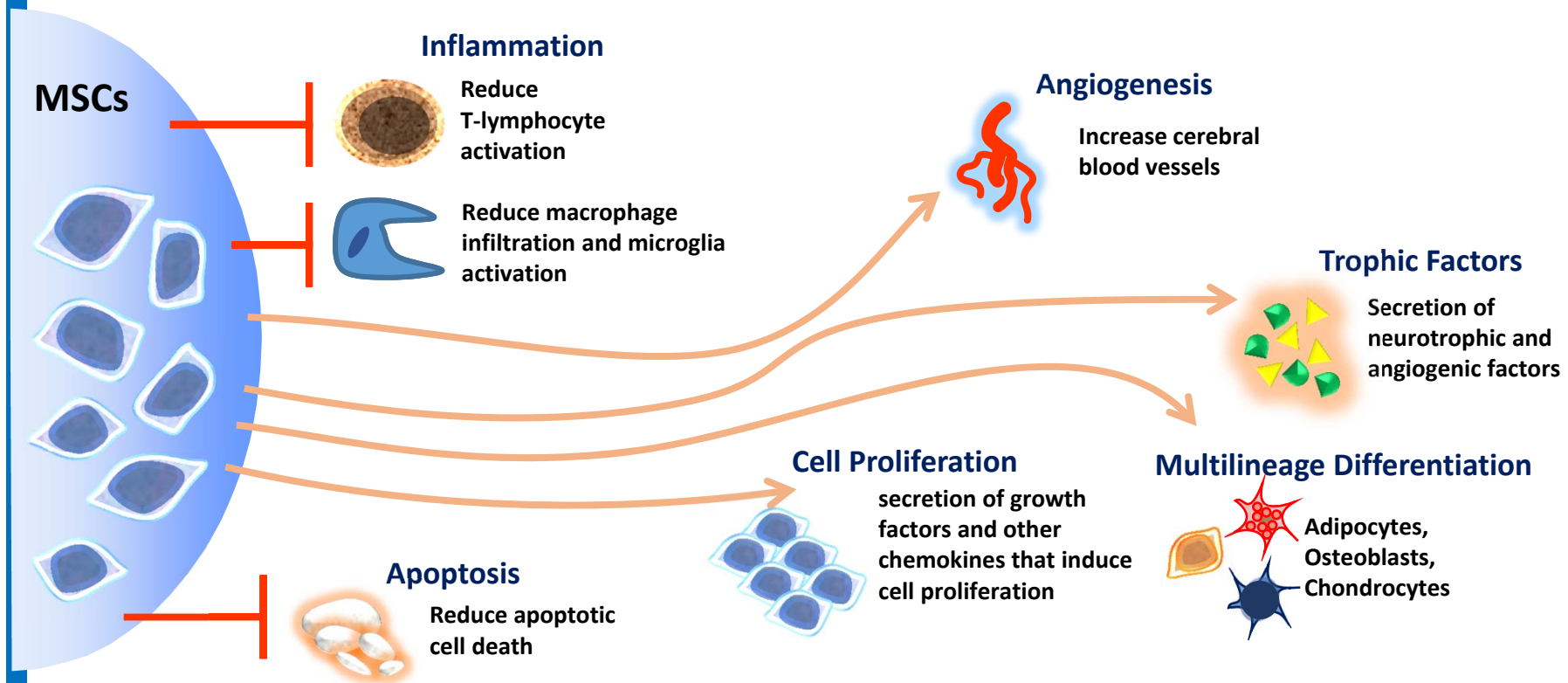
- ✓ **in vivo-like tissue organization:** fibroblast are distributed around tumour aggregates
Light sheet fluorescence microscopy (LSFM)



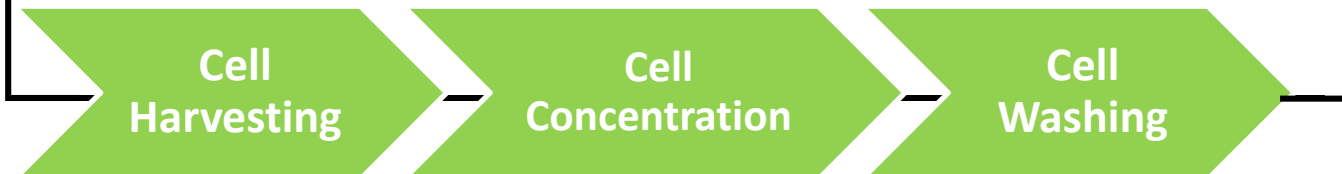
- i. Introduction (Biomanufacturing challenges)
- ii. Goals
- iii. Results - USP of hMSC :
 - i. Overview
 - ii. Continuous Perfusion and Semi-continuous operation modes
 - iii. hMSC's Secretome
- iv. Results - DSP of hMSC :
 - i. Overview
 - ii. Cell concentration
 - iii. Cell washing
 - iv. Process integration



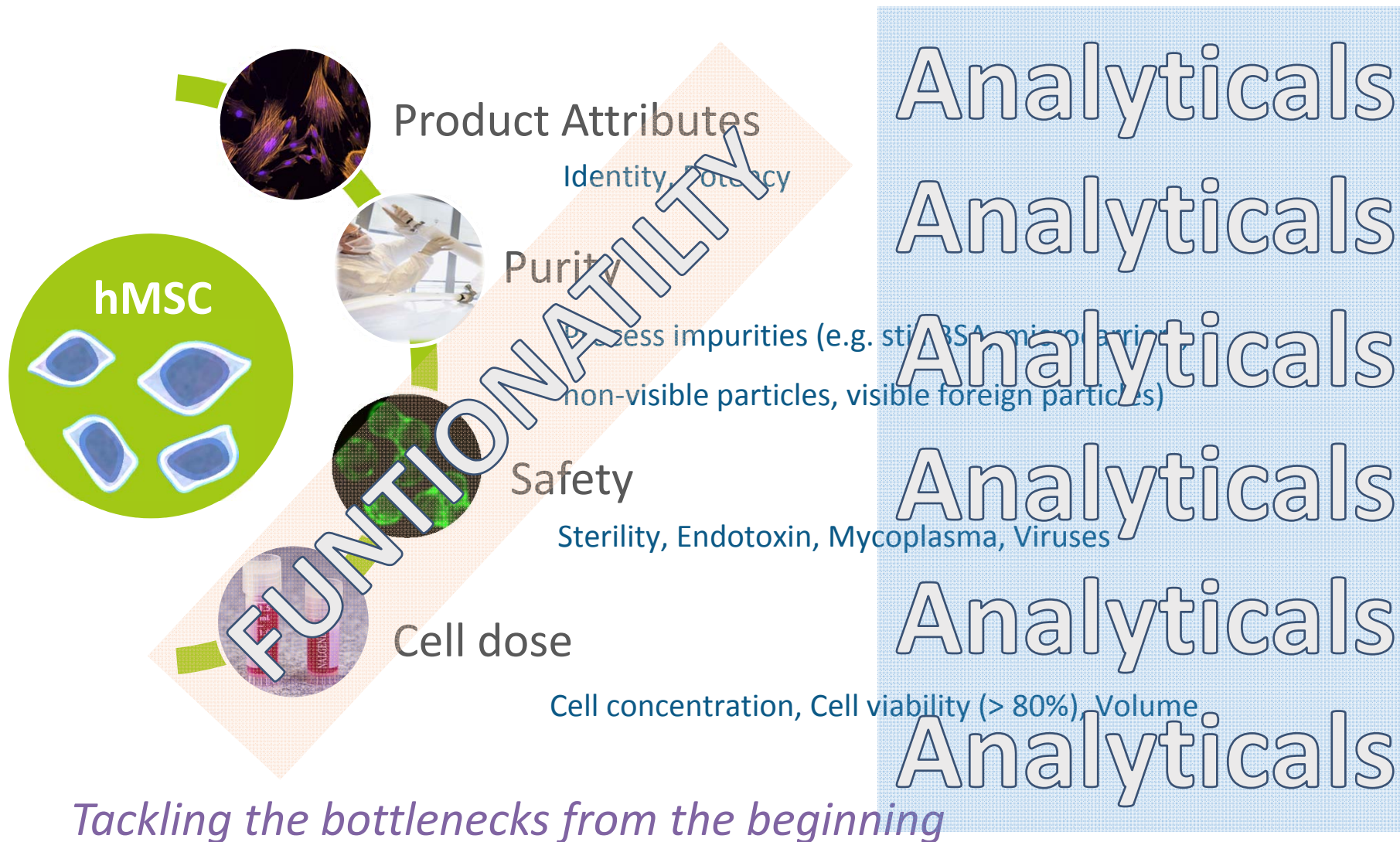
Human Mesenchymal Stem Cells (hMSC) have become key candidates for autologous and allogeneic therapies



Treatment of GvHD, myocardial infarction, stroke, ...

**UPSTREAM PROCESS****PROCESS DURATION****2 - 5 weeks****DOWNSTREAM PROCESS****2 - 6 hours****FILL/FINISH****2 - 6 hours**

Process time impacts “cell enviromes” and thus Cell (=PRODUCT) attributes

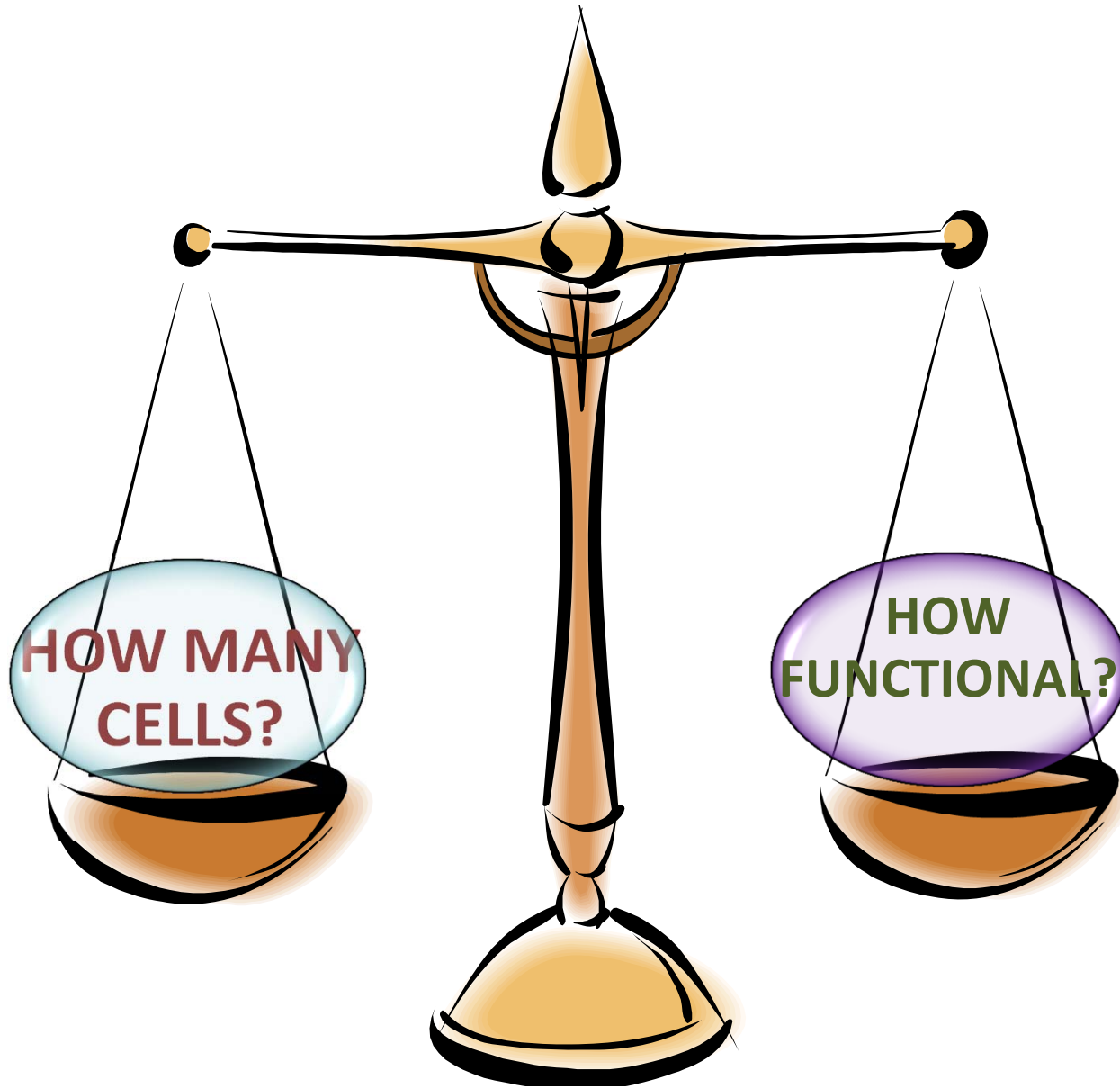


Integrated

Scalable

Robust

GMP compliant





Exploring continuous and integrated strategies for the up- and downstream processing of human mesenchymal stem cells



Increase hMSC volumetric productivities using microcarrier technology and stirred tank bioreactors



Exploring continuous and integrated strategies for the up- and downstream processing of human mesenchymal stem cells



Increase hMSC volumetric productivities using microcarrier technology and stirred tank bioreactors



Establish a scalable clarification process for the removal of microcarriers



Exploring continuous and integrated strategies for the up- and downstream processing of human mesenchymal stem cells



Increase hMSC volumetric productivities using microcarrier technology and stirred tank bioreactors



Establish a scalable clarification process for the removal of microcarriers



Develop filtration-based concentration and washing processes for the downstream processing of hMSC



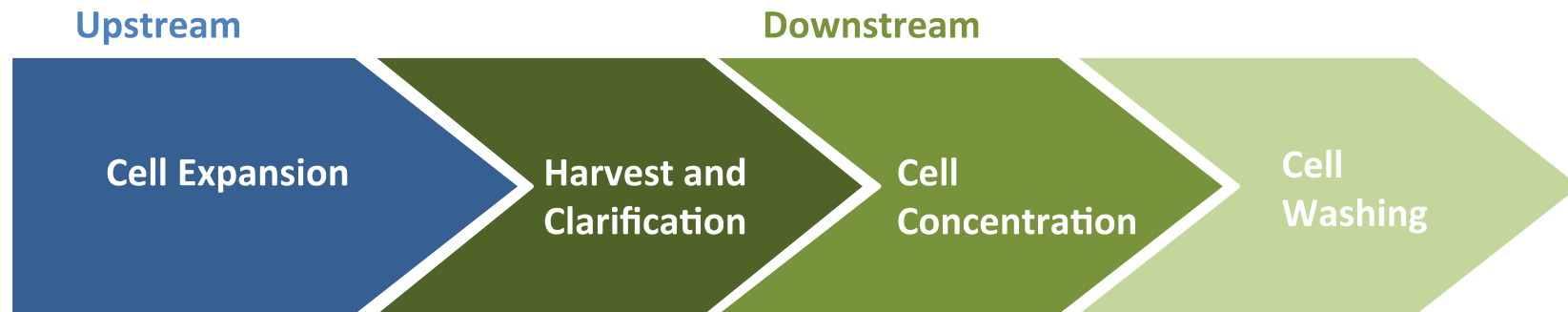
Exploring continuous and integrated strategies for the up- and downstream processing of human mesenchymal stem cells



Integration of up and downstream operations



Aiming to rationally integrate upstream and downstream operations



Process parameters evaluated:

- Bioreactor
- Operation mode

- Membrane's material
- Pore size

- Membrane's material
- Pore size
- Initial cell concentration
- Shear rate
- Permeate flux
- Operation mode

- Operation mode
- Diafiltration Volumes



iBET

- USP OF hMSC: CELL EXPANSION

Production of hMSCs (different sources: bone marrow, adipose tissue, umbilical cord tissue) (for Autologous and Allogeneic Therapies)

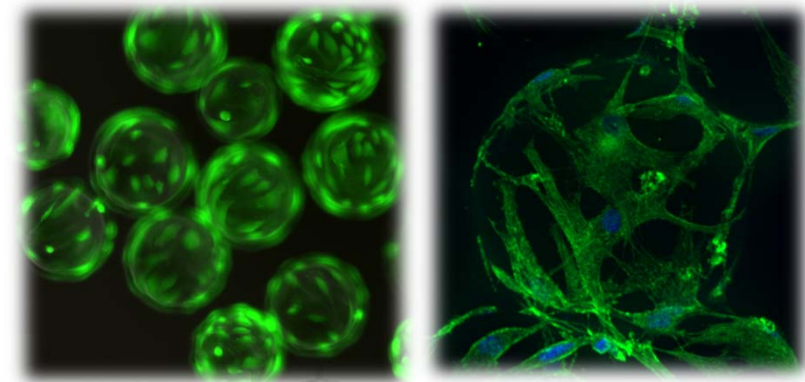


UPSTREAM BIOPROCESSING

AIM: Increase cell volumetric productivities (cell/mL) without compromising cell quality (**viability, identity and potency**)

Bioprocess Development:

- Microcarrier type and concentration
- Culture operation mode (fed-batch, perfusion)
- Environmental conditions (e.g. pO_2)
- Establishment of cGMP compatible processes
- Process scale-up (from 100mL to 2L)



Sousa et al 2015, *Biotechnology Progress*, in press.



Exploring continuous and integrated strategies for the up- and downstream processing of human mesenchymal stem cells



Increase hMSC volumetric productivities using Microcarrier technology and Stirred Tank Bioreactors

Impact of:



Operation Mode

Semi-continuous

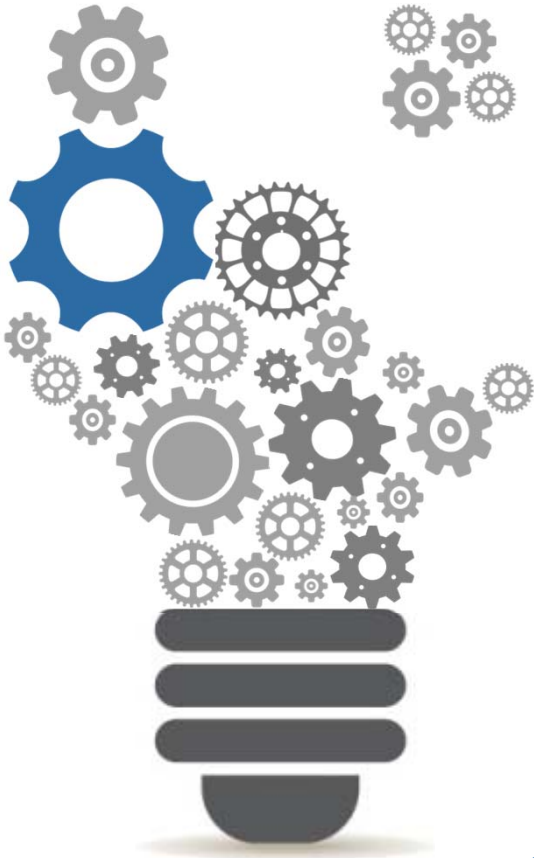
versus

Continuous Perfusion

on hMSC Productivity and Quality

- hMSC volumetric productivities
- hMSC metabolism
- hMSC identity and multipotency
- hMSC secretome

comparison with cells cultured in Planar Technologies (e.g. Tflasks, Cell stacks)

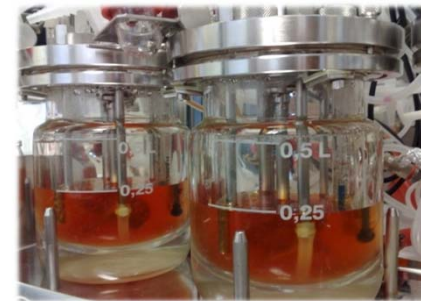
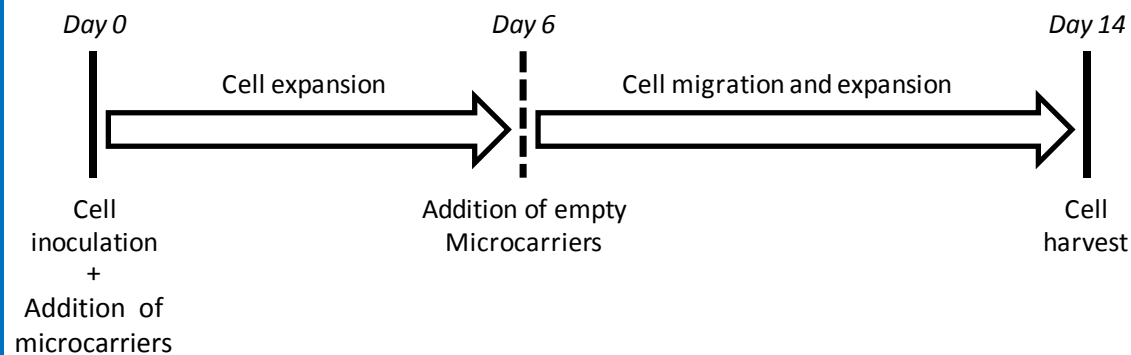




hMSC expansion in xeno-free conditions using Stirred Tank bioreactors

Synthetic Microcarriers: Synthemax® II (Corning)

Xeno-free Culture Medium: MesenCult-XF (Stem Cell Technologies)



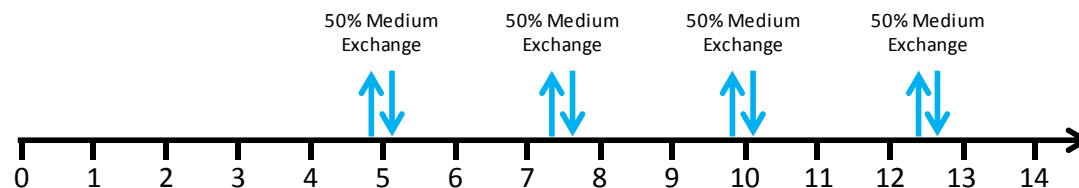
Operation conditions:

(V = 250 mL)

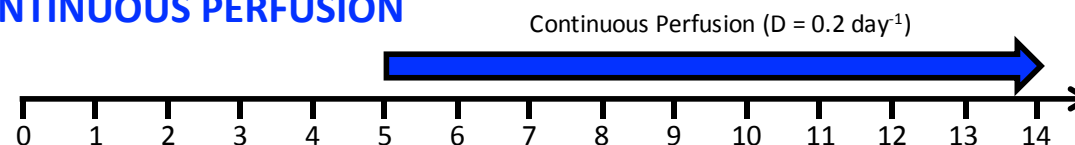
- T = 37 °C
- pO₂ = 4% O₂
- pH = 7.2

Operation Mode

SEMI-CONTINUOUS



CONTINUOUS PERFUSION



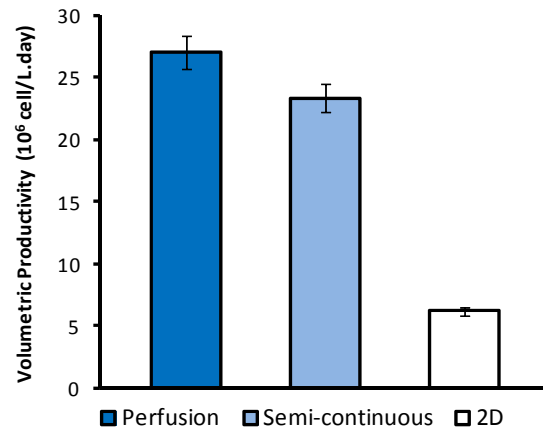
Cell retention device:

ATF™-1 (Alternating Tangential Flow)



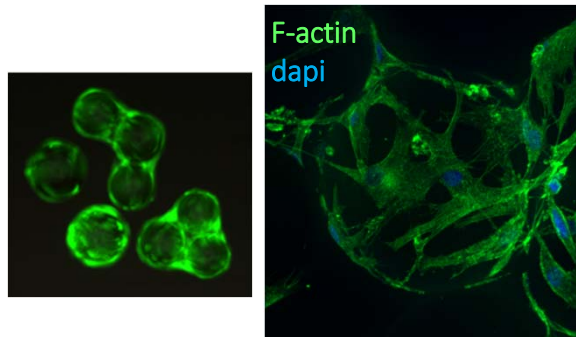
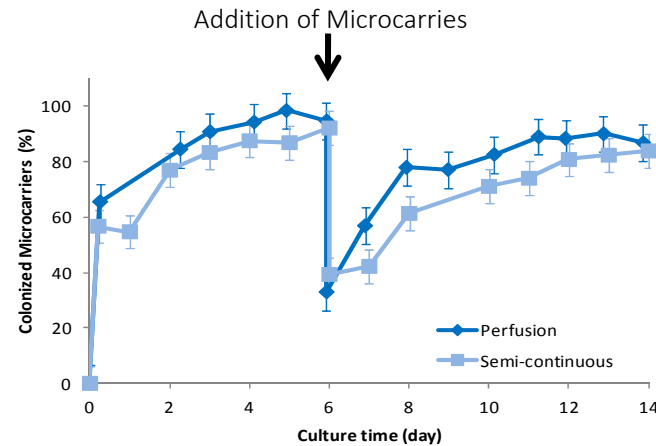


Cell Volumetric Productivities

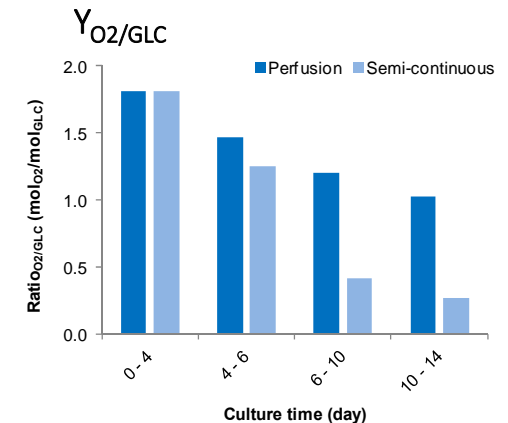
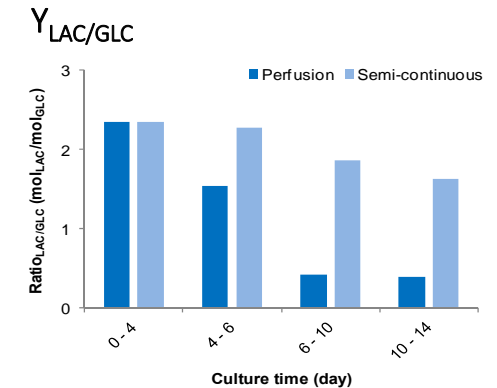


	Microcarrier-based culture in stirred tank bioreactors		Planar (2D) static culture
	Continuous perfusion	Semi-continuous	
X_{max} ($\times 10^5$ cell/mL)	3.4	2.8	1.0
Expansion ratio (X_{max}/X_0)	13.4	11.2	4.1

Microcarrier Colonization



Cell Metabolism

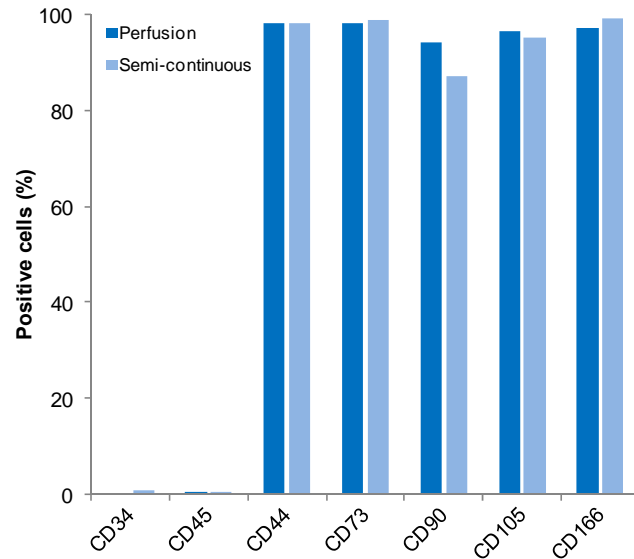


- ✓ Higher X_{max} , expansion ratio and cell volumetric productivity in Bioreactors operating in continuous perfusion
5-fold improvement in cell volumetric productivities when compared to planar technologies (2D)
- ✓ More efficient microcarrier colonization in Bioreactors operating in continuous perfusion
- ✓ Metabolic shift in Bioreactors operating in continuous perfusion: Anaerobic glycolysis → Oxidative phosphorylation



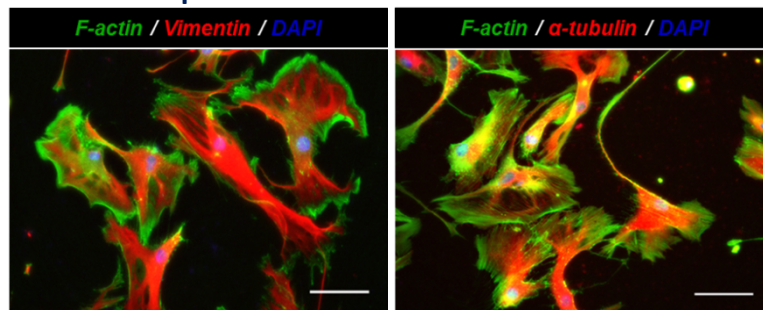
hMSC Characterization

- Identity

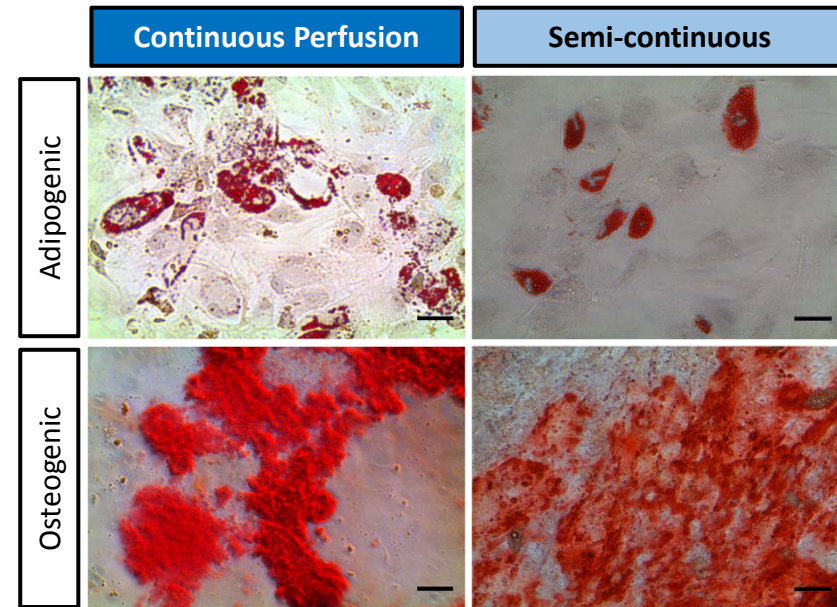


- Morphology

hMSCs expanded in bioreactors operating in continuous perfusion



- Differentiation potential



- ✓ After expansion in bioreactors operating in continuous perfusion, cells maintained their **identity**, **morphology** and **differentiation potential**.
- ✓ No differences were observed between all culture strategies/systems evaluated

AIM: Develop a proteomics toolbox to better characterize hMSC and unveil differences in hMSC's secretome when cells are expanded in planar or bioreactor conditions

Planar



Cell Expansion

Bioreactors

Continuous Perfusion
Semi-Continuous



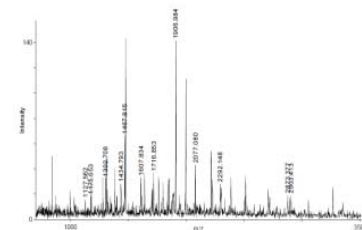
Fractionation Step

NanoLC

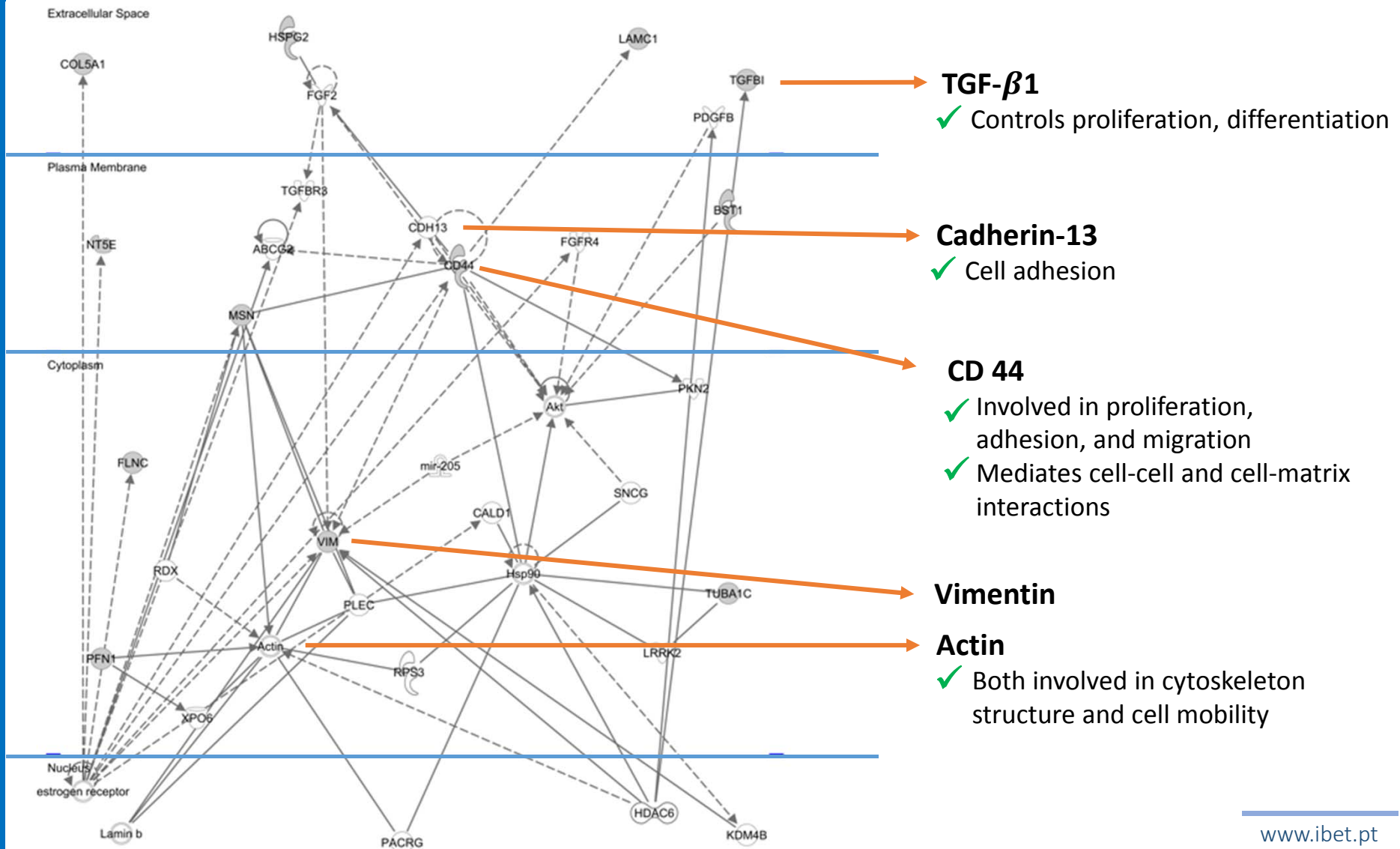
Mass spectrometry analysis

ESI-TripleTOF 6600 (ABSciex)

Protein
Identification

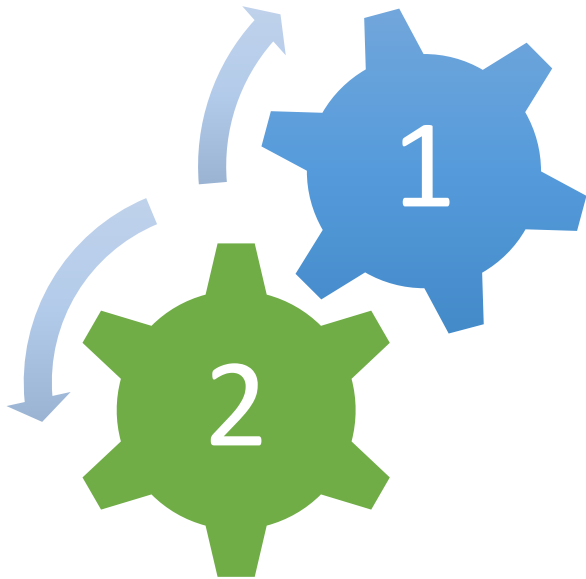


E.g.: Top network related with Cellular Movement



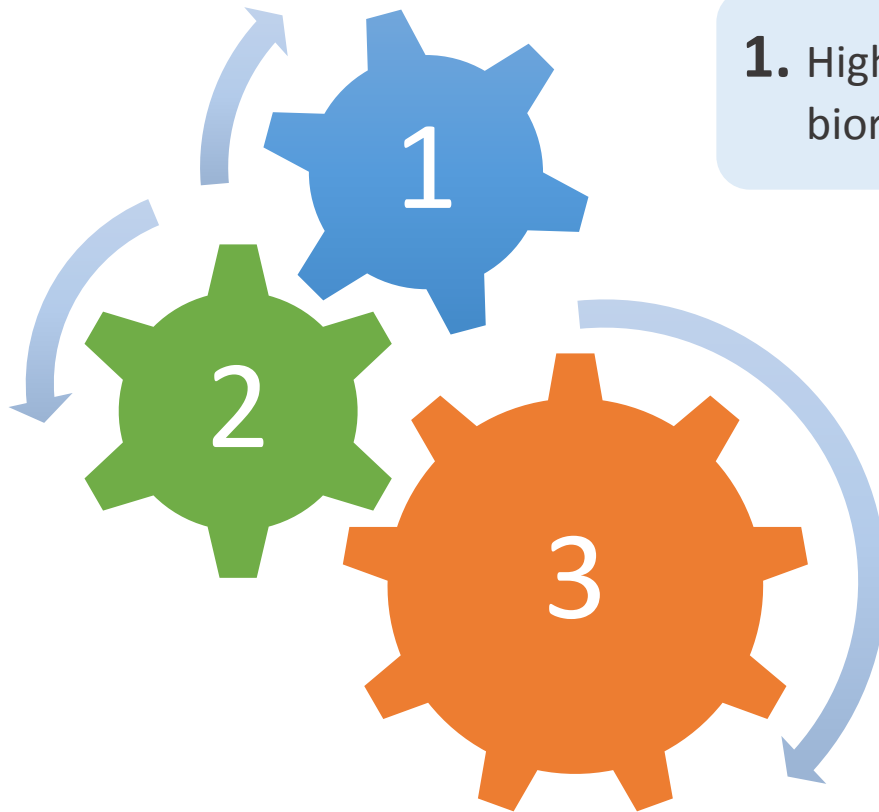


- 1.** Higher X_{max} , expansion ratio and productivity on bioreactors (specially perfusion operation mode)



1. Higher X_{max} , expansion ratio and productivity on bioreactors (specially perfusion operation mode)

2. **Metabolic shift** in perfusion culture towards oxidative phosphorylation



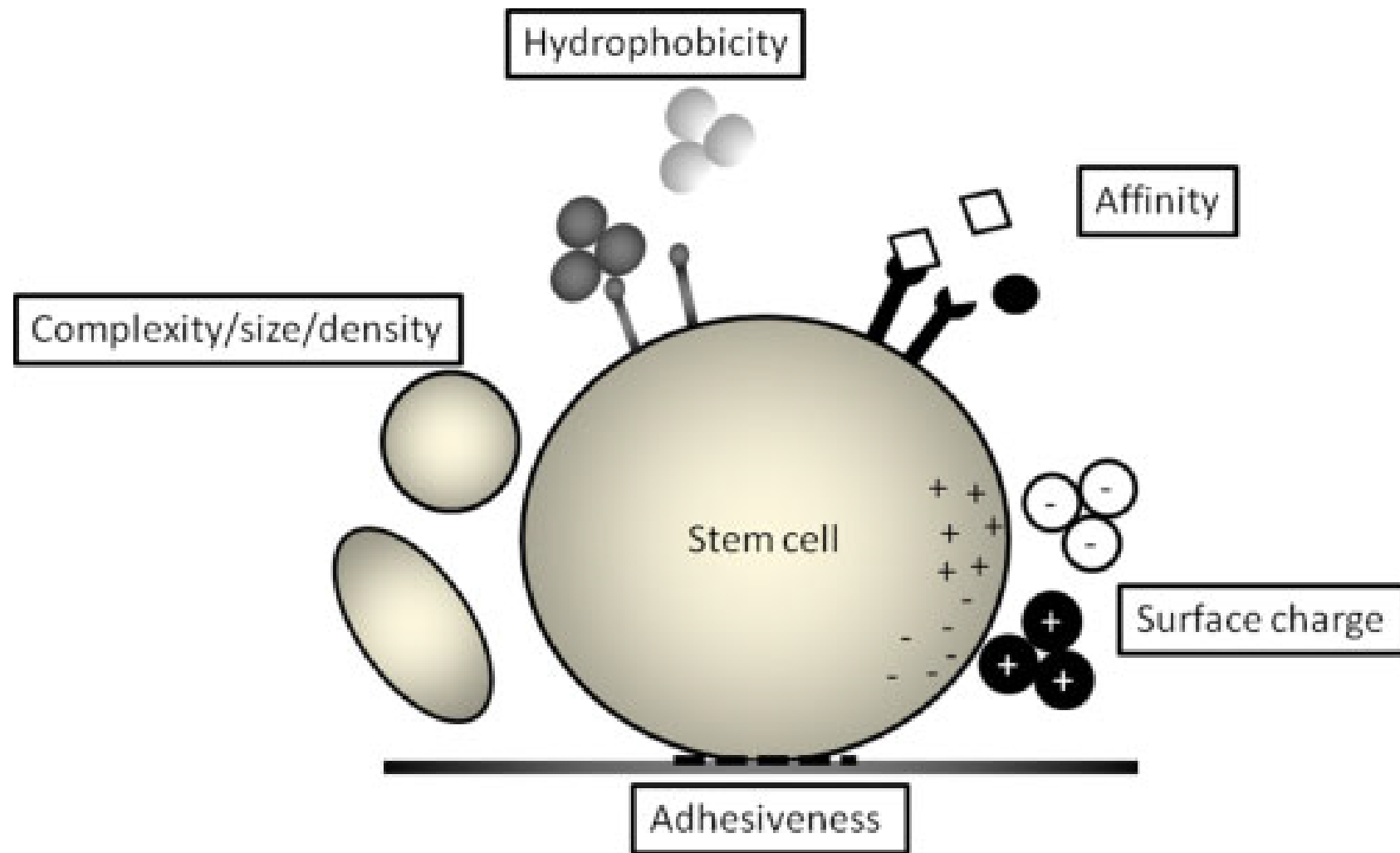
1. Higher X_{max} , expansion ratio and productivity on bioreactors (specially perfusion operation mode)

2. **Metabolic shift** in perfusion culture towards oxidative phosphorylation

3. hMSC's secretome: Bioreactors' environment leads to higher proliferation, cell migration, promote cell-to-cell signaling and representation of angiogenesis and production of growth factors – **better characterization of hMSC**

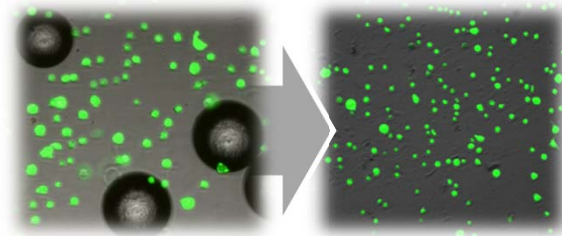
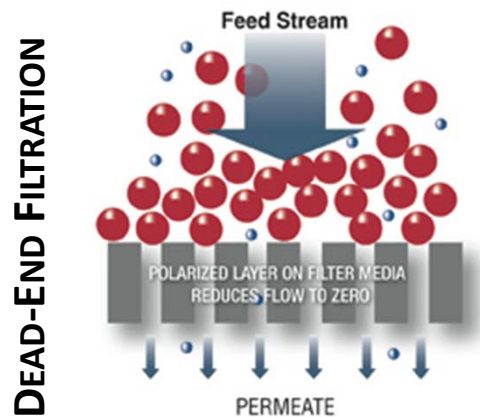


Properties of Stem Cells that can be exploited during separation process





AIM: Microcarrier removal

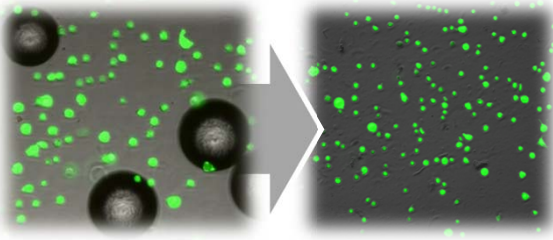


Cell Concentration = 2×10^5 cell/mL
Cell Size: $> 15 \mu\text{m}$
Microcarriers' size $> 120 \mu\text{m}$

Impact on:

- Mesh material
- Pore size

- ✓ Cell viability
- ✓ Cell recovery yields

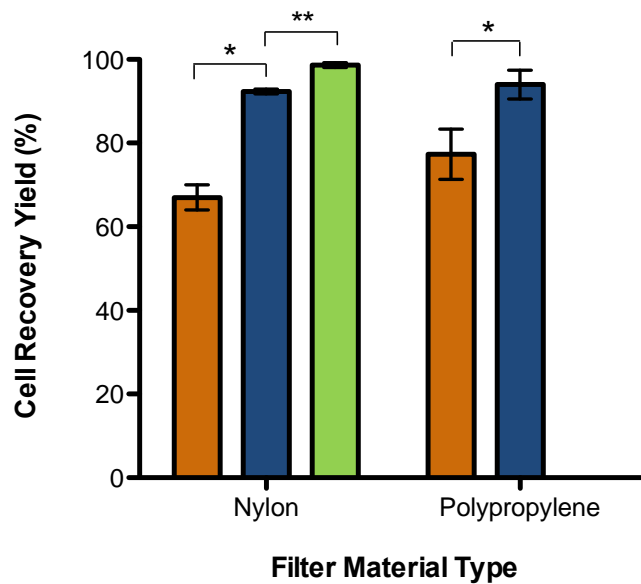


Cell Concentration = 2×10^5 cell/mL

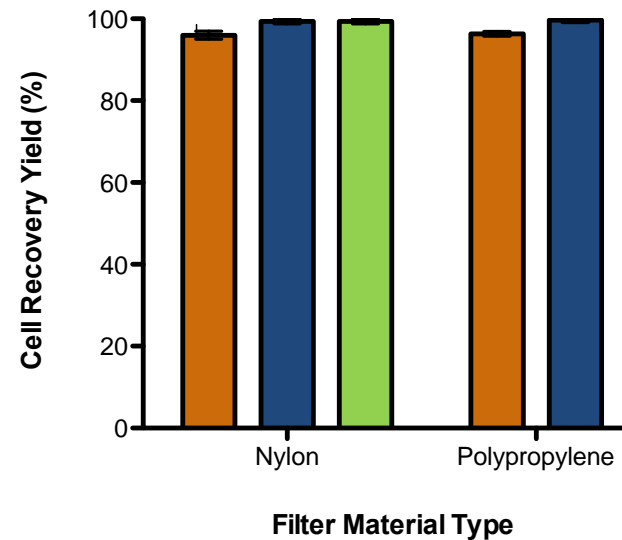
Cell Size: $> 15 \mu\text{m}$

Microcarriers' size $> 120 \mu\text{m}$

Cell Recovery Yields



Cell Viability



Filter pore size:

30 μm

80 μm

100 μm

- ✓ Higher filter pore sizes yield higher cell recoveries
- ✓ No differences observed in cell viability ($>98\%$) and recovery yields ($>92\%$) between the materials
- ✓ Efficient microcarrier removal in all tested strategies (confirmed by microscopic evaluation)



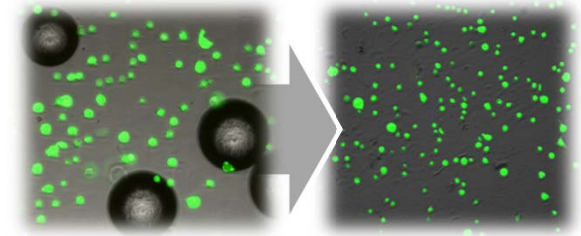
Evaluation of scalable strategies for microcarrier removal

“Scaling-up”: from 0.2 to 2 L

Towards an integrated bioprocess for hMSC manufacturing



OptiCap® XL 1 Capsules (EMD Millipore)
(polypropylene, >75 µm pore size)



Scale	Cell Recovery (%)	Cell Viability (%)
0.2 L	> 90%	> 95%
2 L	94%	98%

✓ **Cell recovery yields and viability** were maintained after scale-up

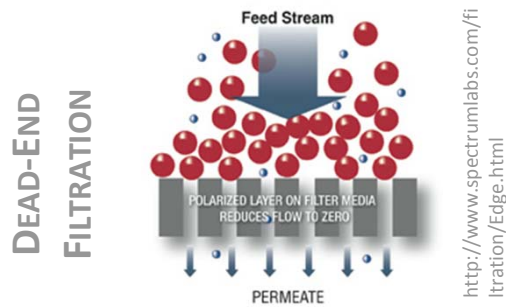


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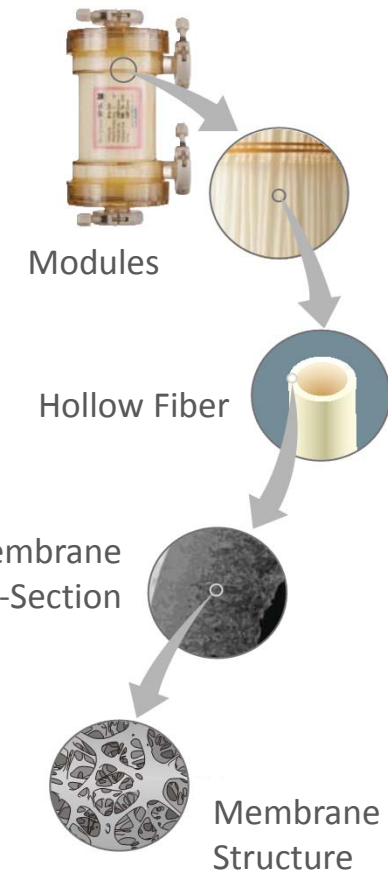
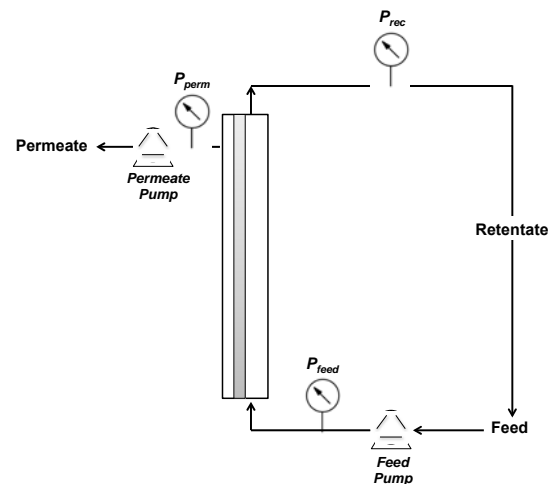
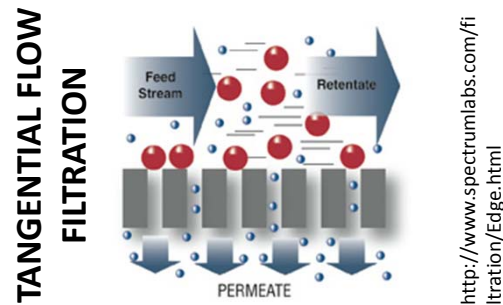
- DSP of hMSC: CELL CONCENTRATION



AIM: Microcarrier removal

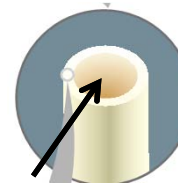


AIM: Volume Reduction

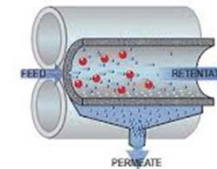




Impact of the shear rate on the concentration process:



ys://www.ak-bio.com



$$\gamma = \frac{4 Q}{\pi r^3}$$

**Inlet
Flux
($\text{m}^2 \cdot \text{h}^{-1}$)**

**Cell Viability (%)
VRF=4**

**Cell Rec. Yield
(%), VRF=4**

175	85	38
375	92	62
750	95	92

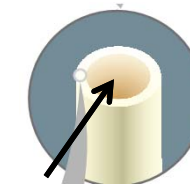
Volume Reduction Factor

- **Higher shear rates (3000 s^{-1}):** Recovery of higher number of viable cells



Impact of the shear rate on the concentration process:

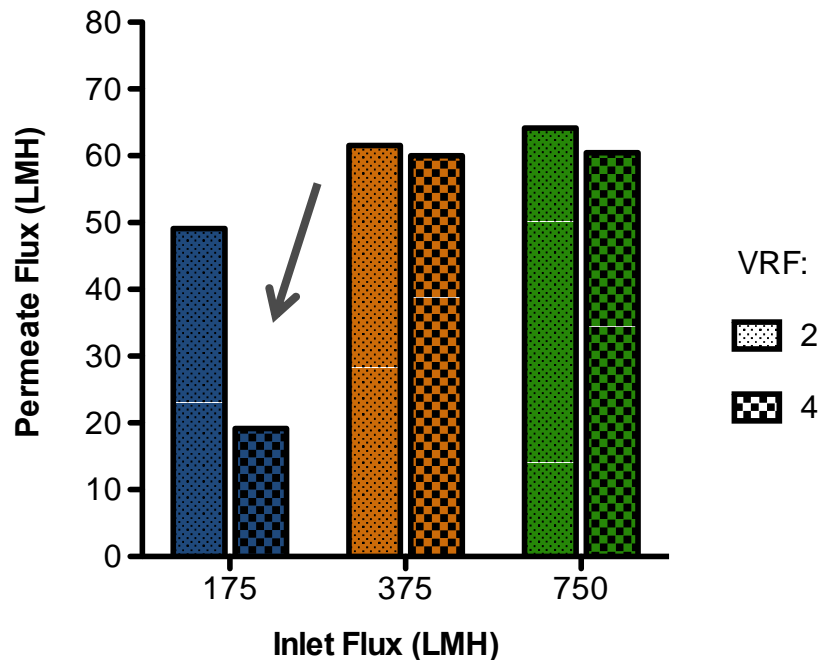
700 s⁻¹ = 175 LMH 1500 s⁻¹ = 375 LMH 3000 s⁻¹ = 750 LMH



$$\gamma = \frac{4 Q}{\pi r^3}$$

<https://www.ak-bio.com>

Permeate Flux



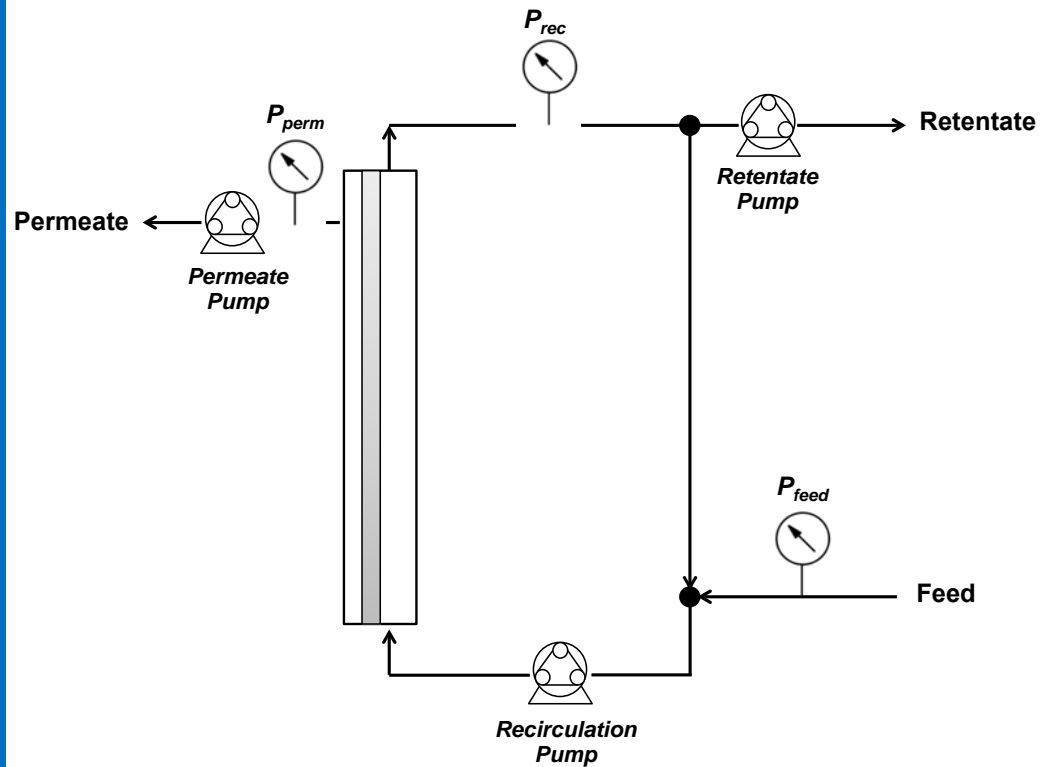
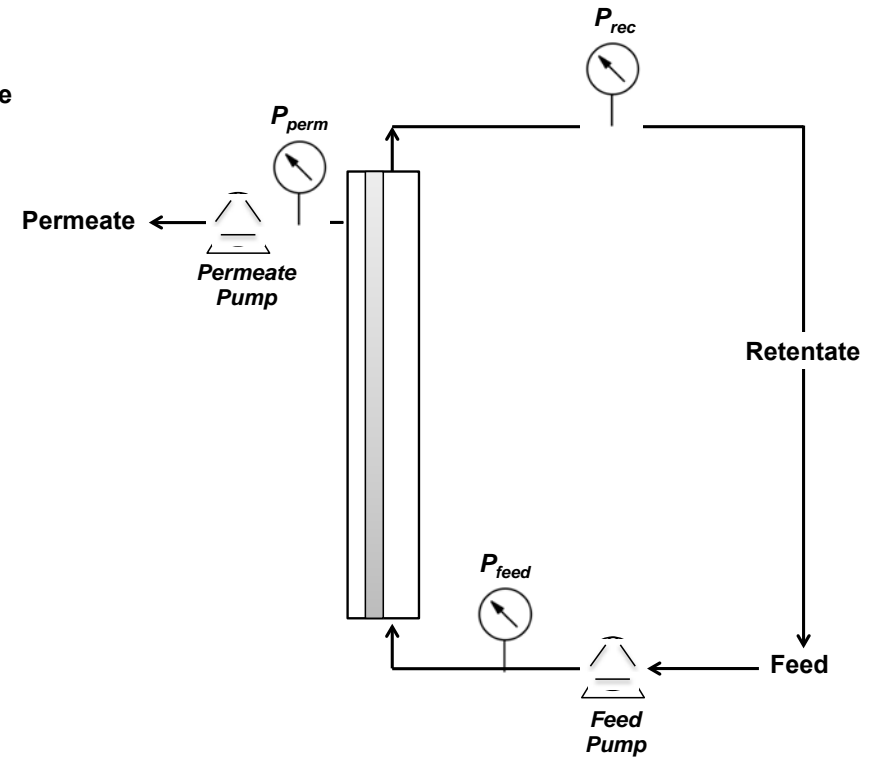
Cell Lysis

LDH activity (U/mL)

X Lower shear rates (700 s⁻¹): decline on the permeate flux over time, leading to irreversible fouling and increase in cell death – higher residence time

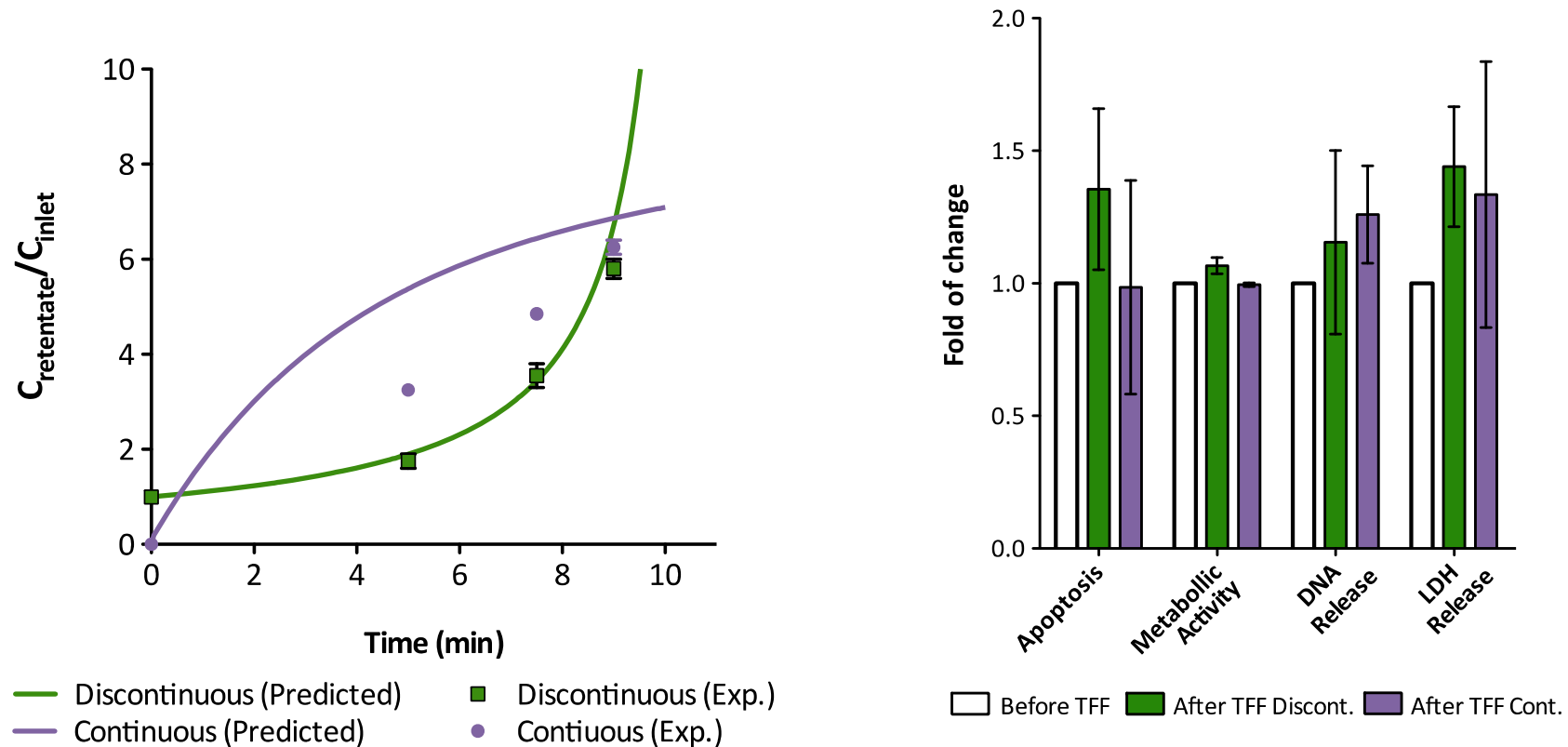


Impact of the operation mode (Continuous and Discontinuous TFF):

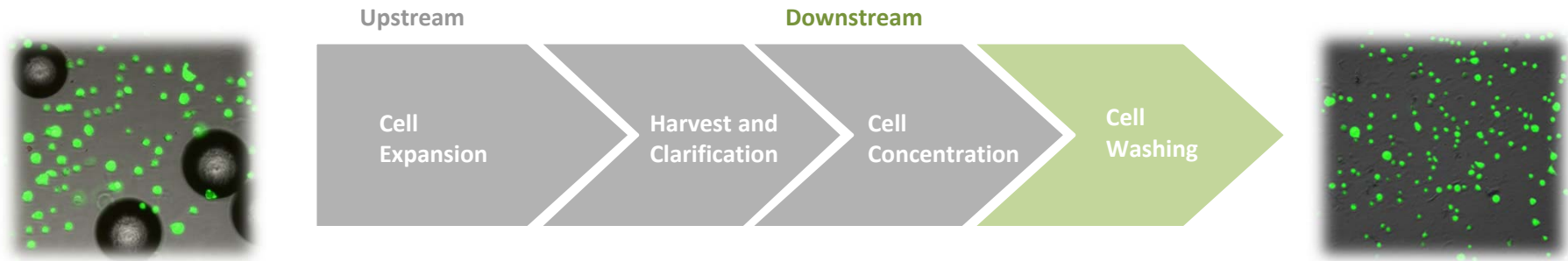
CONTINUOUS TFF**DISCONTINUOUS TFF**



Impact of the operation mode (Continuous and Discontinuous TFF):

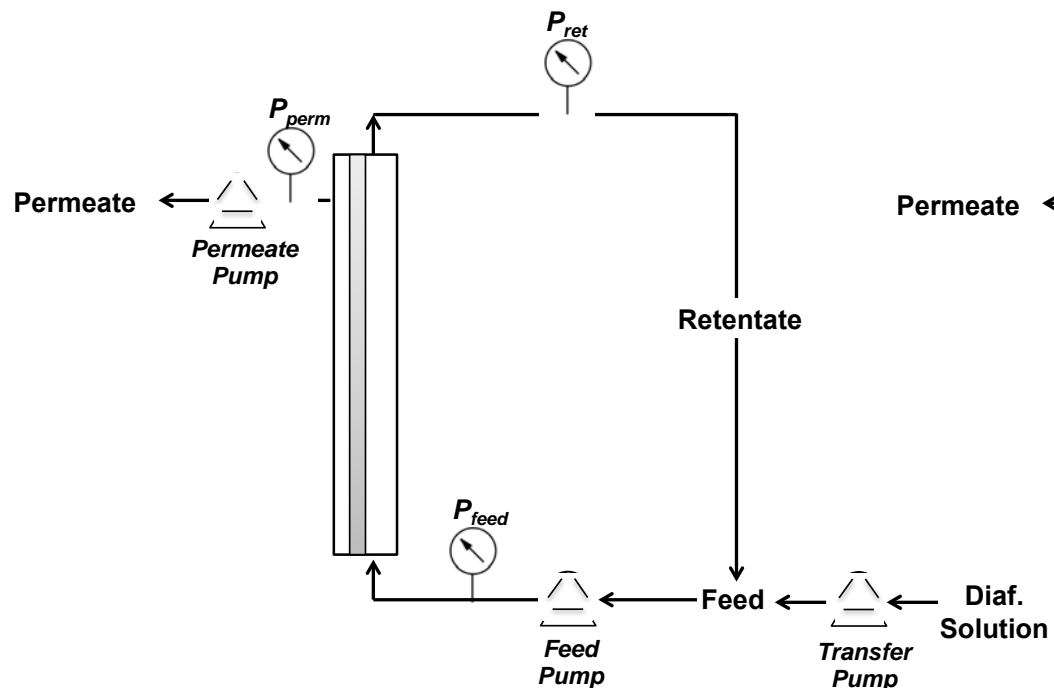


- ✓ **Both operation modes:** No impact on cell recovery yield (80%)
- ✓ **Continuous TFF:** higher concentration factors were achieved sooner however for **process integration** (using the same device) only **discontinuous** is suitable.

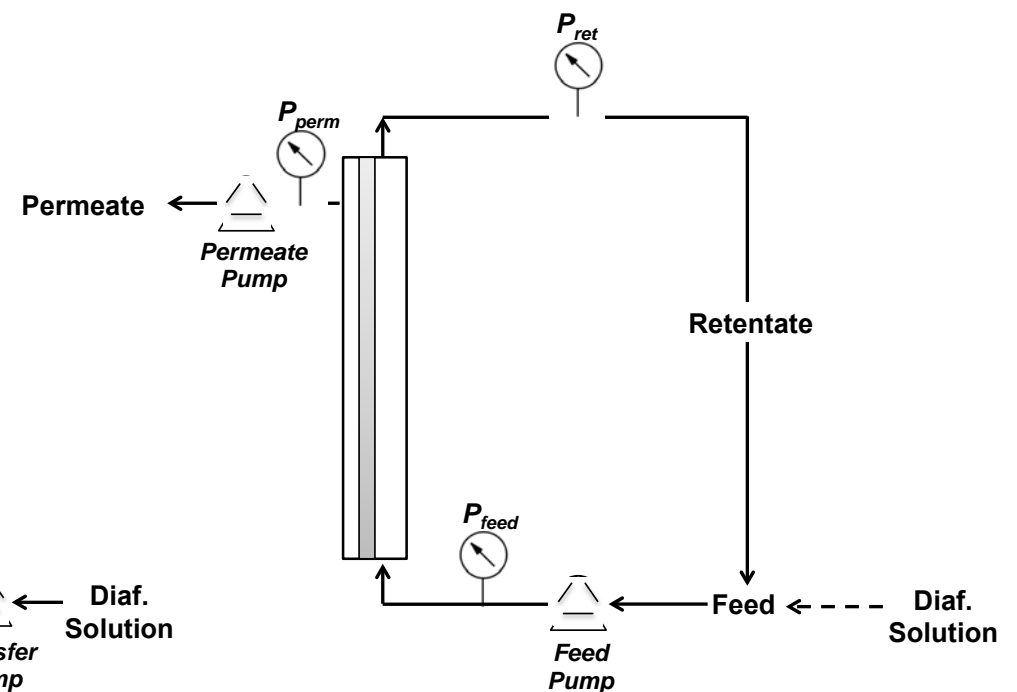


AIM: Protein Removal

CONTINUOUS DIAFILTRATION



DISCONTINUOUS DIAFILTRATION





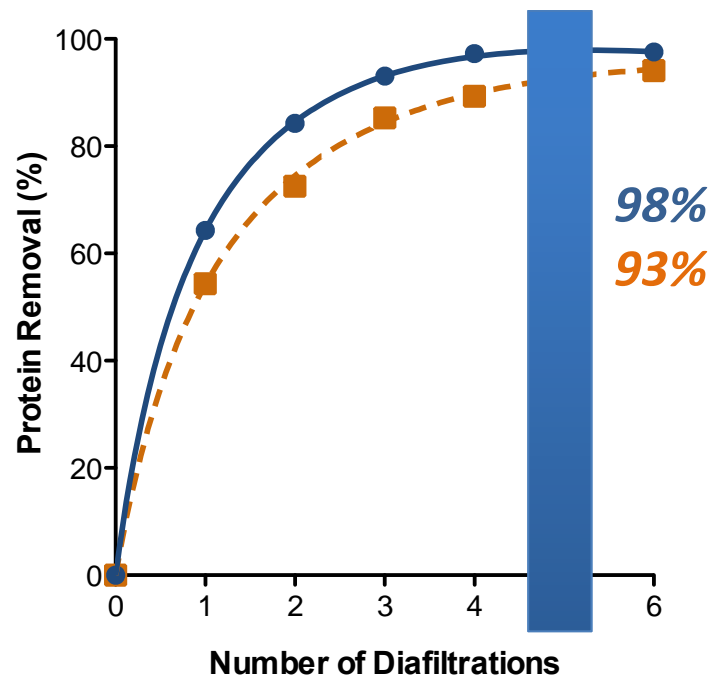
*Impact of different operation modes of TFF on protein removal and cell recovery yield
(high protein clearance, high cell recoveries, high viability, QA)*

CONTINUOUS DF

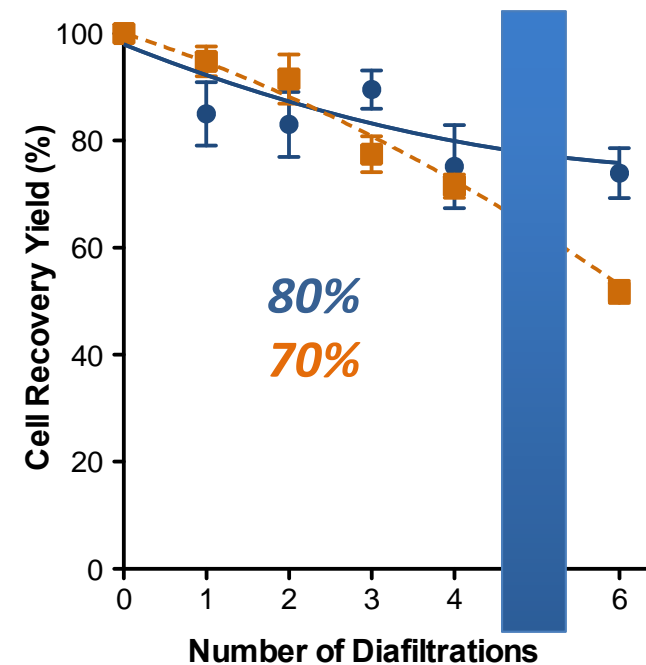
DISCONTINUOUS DF

Concentrated cell suspension
DMEM + 10% FBS
DF with DPBS

Protein Clearance



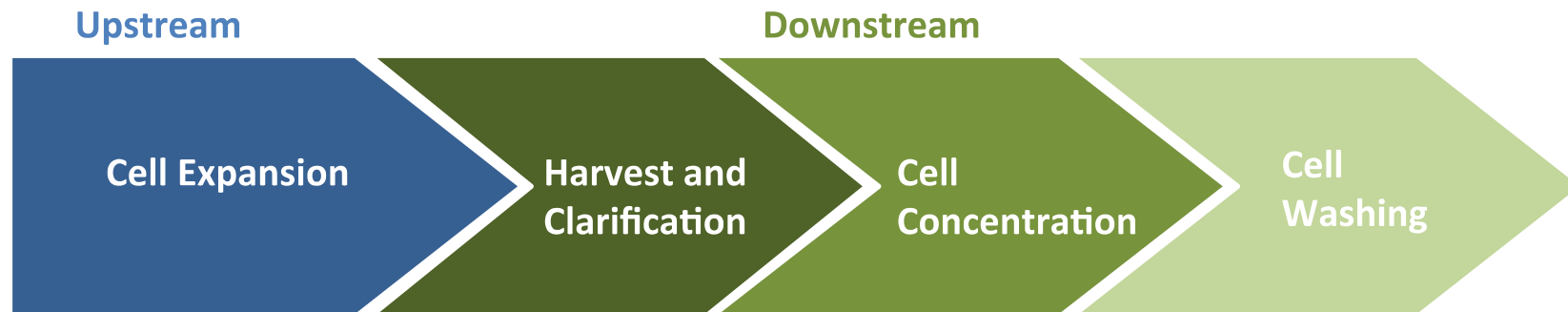
Cell Concentration



✓ **Continuous Diafiltration:** Higher protein clearance (98%) and cell recovery yield (80%)



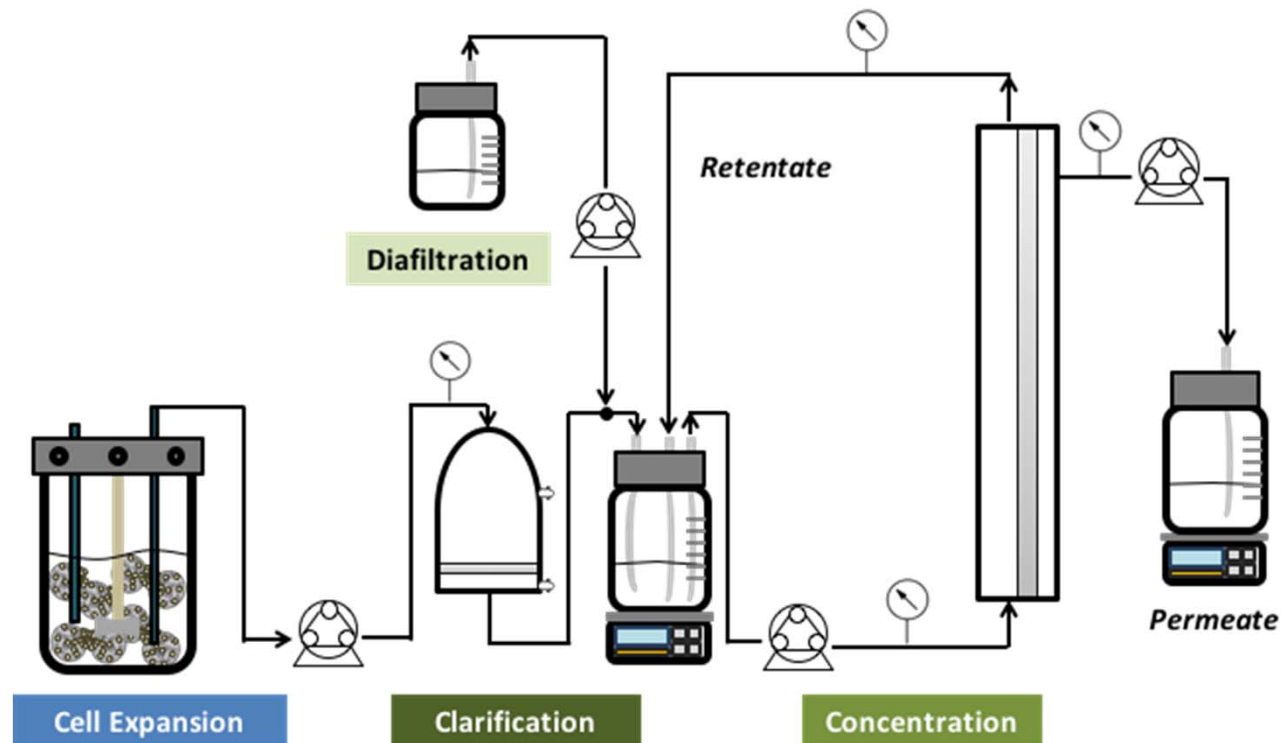
Aiming to rationally integrate upstream and downstream operations



- | | | | |
|---|---|---|---|
| ■ Operation mode
Continuous
Perfusion | ■ Membrane's material
Polypropylene
■ Pore size
> 75 μm | ■ Membrane's material
Polysulfone
■ Pore size
> 0.45 μm
■ Initial cell concentration
> 2×10^5 cell/mL
■ Shear rate
3000 s^{-1}
■ Permeate flux
250 LMH
■ Operation mode
Discontinuous TFF | ■ Operation mode
Continuous DF
■ Diafiltration Volumes
5 DVs |
|---|---|---|---|

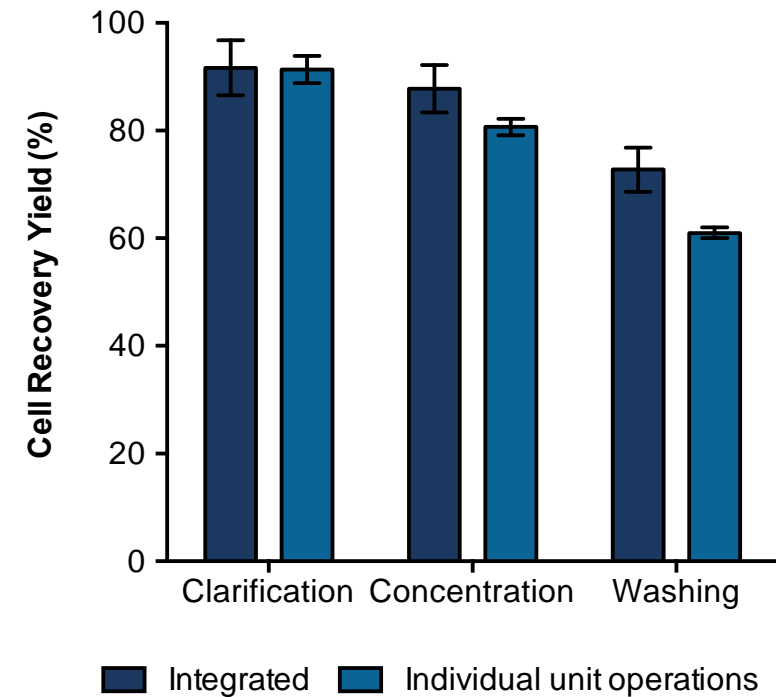
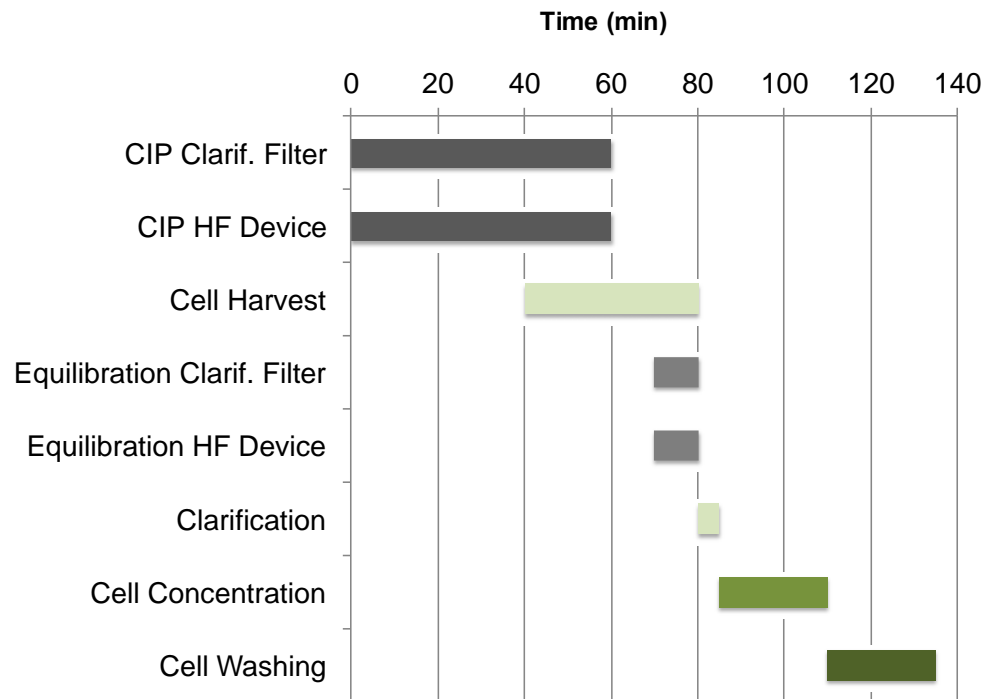


Aiming to rationally integrate upstream and downstream operations



Integration:

Closed system, resulting in the elimination of hold steps and decreasing the equip. footprint

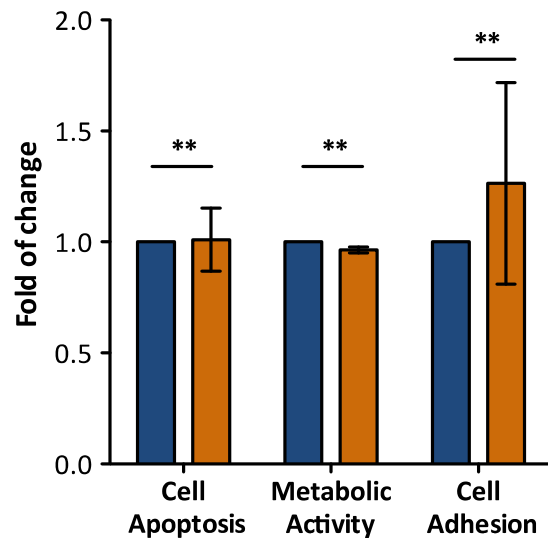
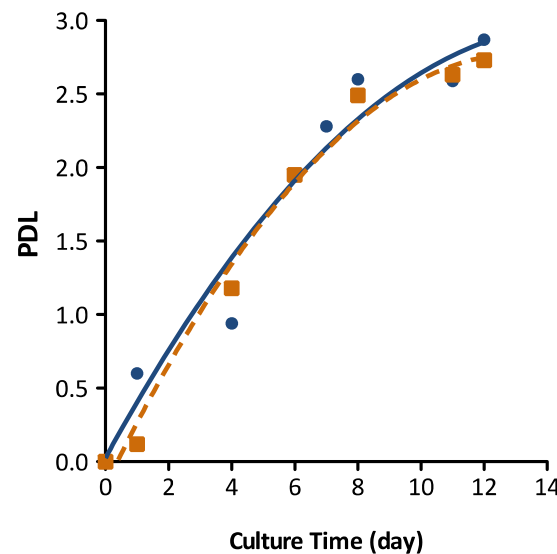
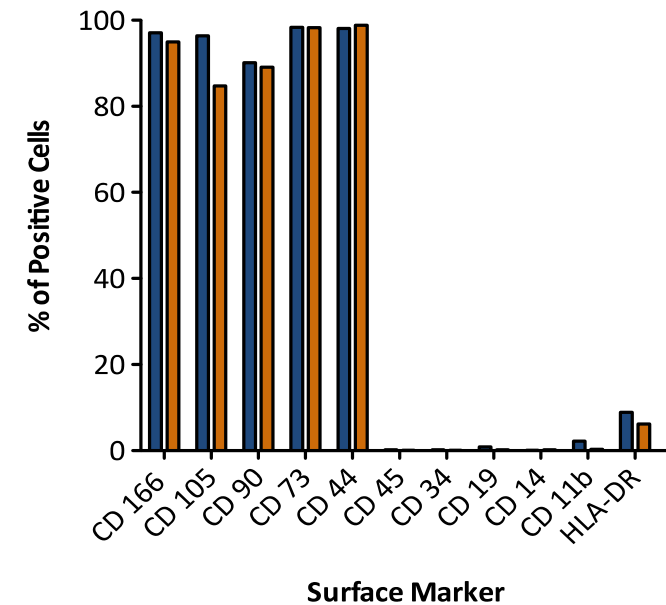
**VRF = 10X; 5 DVs**

- ✓ **Faster** processing after cell expansion (1,5 h)
- ✓ **Cell Recovery Yield:** More than 70% of hMSC, with viability > 95%
(10% more than having separate operations)



AFTER USP

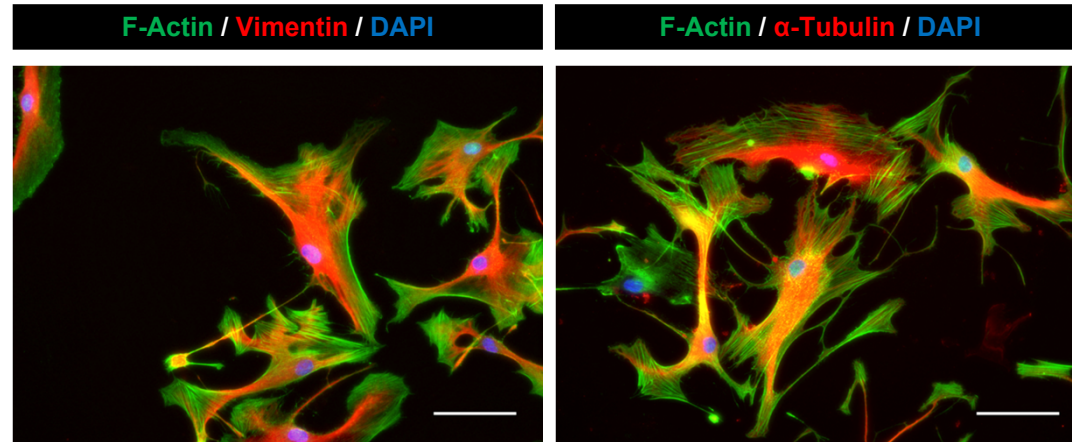
AFTER DSP

Apoptosis and metabolic activity***Proliferation Capacity******Cell Identity***

- ✓ hMSC maintained their immunophenotype and metabolic activity after processing;
- ✓ Ability to adhere to plastic surfaces and proliferative capacity (PDL = 3) after re-plating

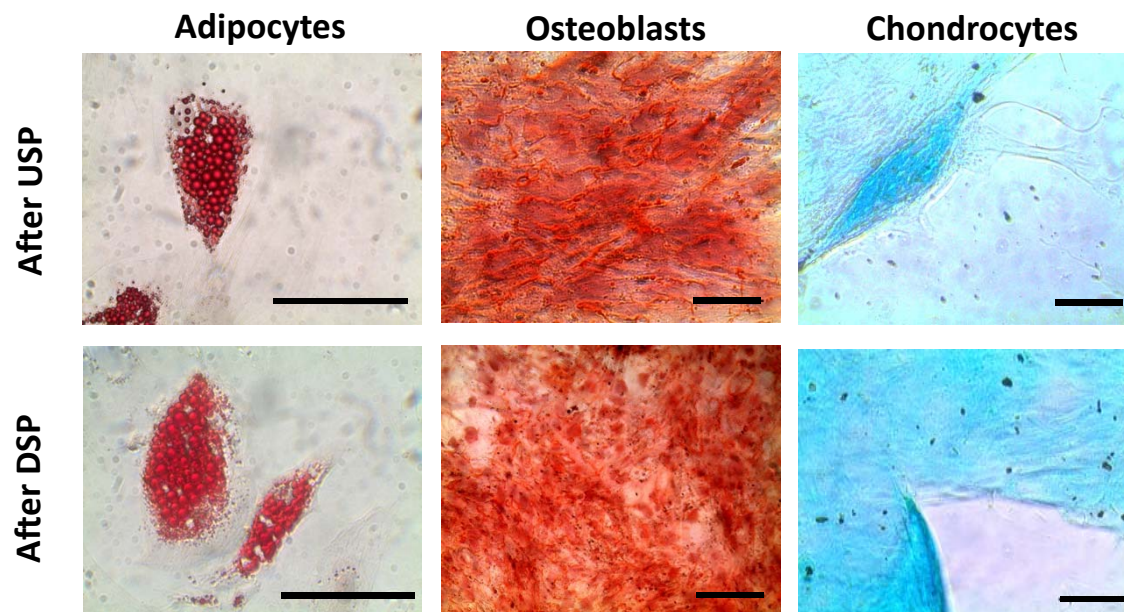


Morphology

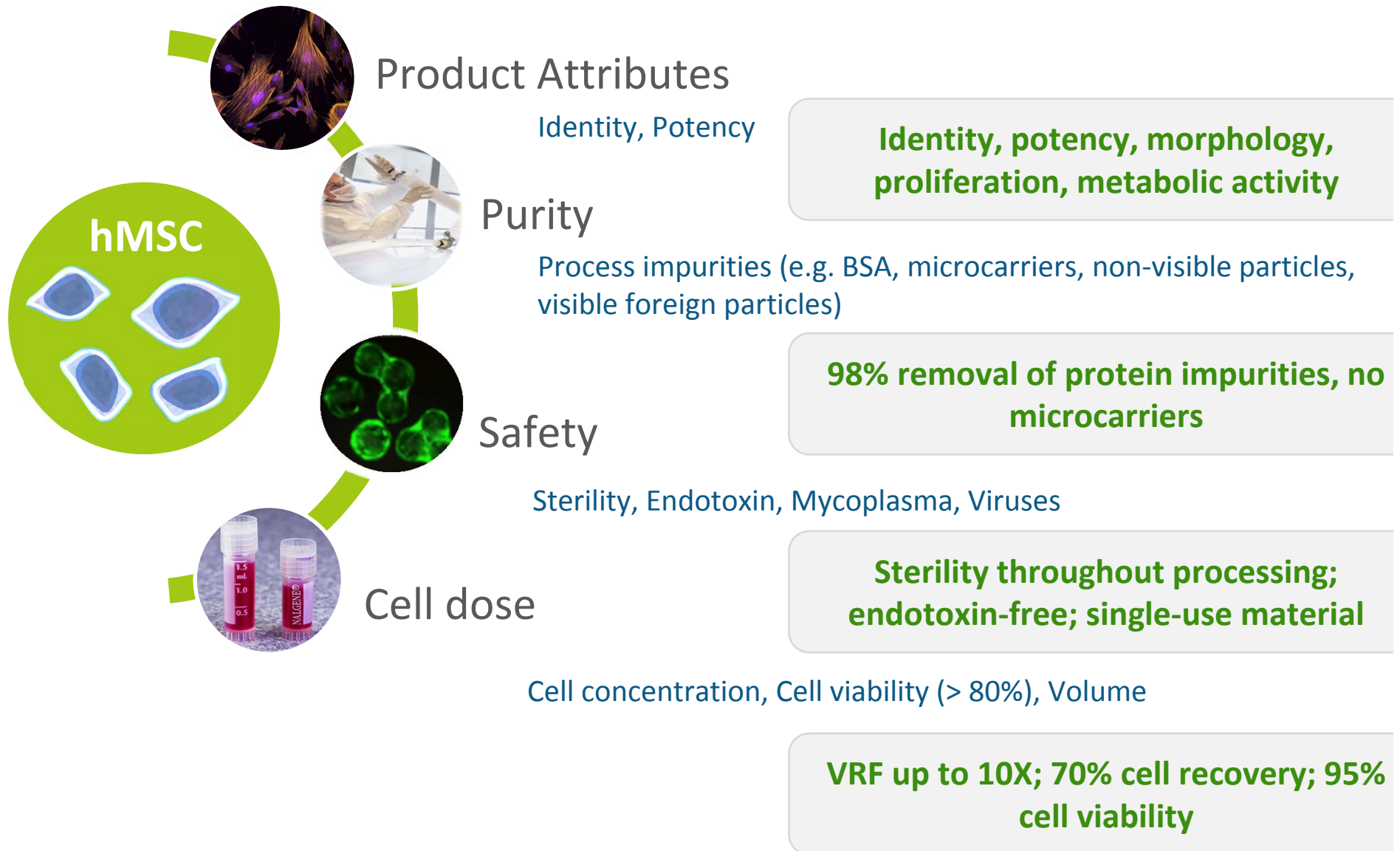


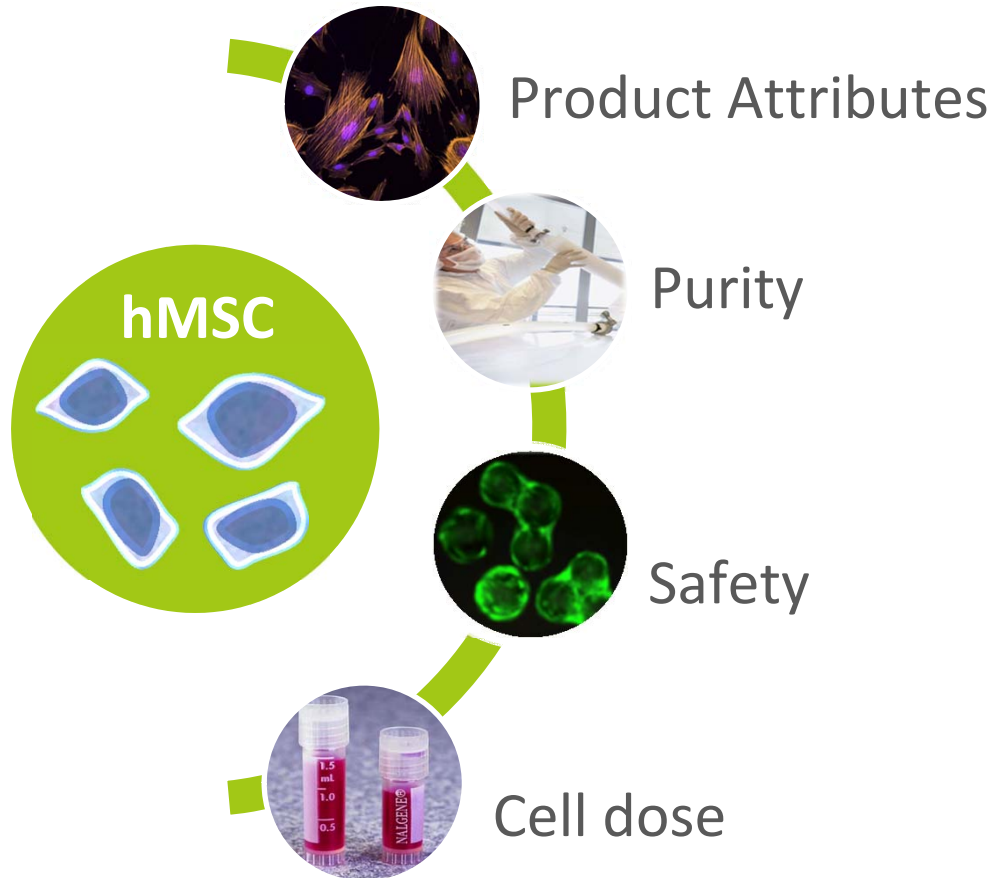
Morphology and adhesion:
hMSC successfully re-acquire their
typical spindle-like morphology
with organized actin fibers

Differentiation Potential



Potency:
hMSC maintained their
multilineage differentiation
potential





Tackling the bottlenecks from the beginning

*Robust
Scalable
Integrated
Clinical-grade*

DSP:

- ✓ Applicability for both autologous and allogeneic therapies (scale-out and scale-up)
- ✓ Valid for other stem cell types relevant for the cell therapy industry (e.g. hiPSC)



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- ACKNOWLEDGEMENTS

Animal Cell Technology Unit

www.ibet.pt/research/animal-cell-technology



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Thank you

“The cell therapy industry has an opportunity to learn from protein processing and anticipate Upstream & DSP bottlenecks by proactively developing technologies to address future scales.”

Adapted from Pattasseril et al (2013)

